Compression device with wear area

A device for applying compression treatment to a part of a wearer’s body has an inner face for being placed adjacent to the part of the wearer’s body in use and an outer face opposite the inner face. The device includes a pressure applicator to apply compression to the wearer’s body part when the device is placed on the wearer’s body part. First and second fastener elements are mounted on the device. The second fastener element is adapted for releasably connecting to the first fastener element for use in holding the device on the wearer’s body part. A visual indicator associated with the second fastener element is adapted to show where to engage the first fastener element with the second fastener element. The visual indicator is adapted to wear upon repeated connection and disconnection of the first and second fastener elements so that the visual indicator fades over time.
Description

FIELD OF THE INVENTION

[0001] The present invention is directed generally to a compression device for applying compression therapy to a body part of a wearer.

BACKGROUND OF THE INVENTION

[0002] A major concern for immobile patients and other persons alike are medical conditions that form clots in the blood, such as, deep vein thrombosis (DVT) and peripheral edema. Such patients and persons include those undergoing surgery, anesthesia, extended periods of bed rest, etc. These blood clotting conditions generally occur in the deep veins of the lower extremities and/or pelvis. These veins, such as the iliac, femoral, popliteal and tibial return deoxygenated to the heart. For example, when blood circulation in these veins is retarded due to illness, injury or inactivity, there is a tendency for blood to accumulate or pool. A static pool of blood is ideal for clot formations. A major risk associated with this condition is interference with cardiovascular circulation. Most seriously, a fragment of the blood clot can break loose and migrate. A pulmonary emboli can form blocking a main pulmonary artery, which may be life threatening.

[0003] The conditions and resulting risks associated with patient immobility may be controlled or alleviated by applying intermittent pressure to a patient's limb, such as, for example, a leg to assist in blood circulation. Known devices have been employed to assist in blood circulation, such as, one piece pads and compression boots. See, for example, U.S. Pat. Nos. 6,290,662 and 6,494,852.

[0004] For example, sequential compression devices have been used, which consist of an air pump connected to a disposable wraparound pad by a series of air tubes. The wraparound pad is placed around the patient's leg. Air is then forced into different parts of the wraparound pad in sequence, acting like a peristaltic pump on the leg and improving venous return.

SUMMARY OF THE INVENTION

[0005] In one aspect of the present invention, a device for applying compression treatment to a part of a wearer's body has an inner face for being placed adjacent to the part of the wearer's body in use and an outer face opposite the inner face. The device generally comprises a pressure applicator to apply compression to the wearer's body part when the device is placed on the wearer's body part. A first fastener element is mounted on the device. A second fastener element is mounted on the device and is adapted for releasably connecting to the first fastener element for use in holding the device on the wearer's body part. A visual indicator is associated with the second fastener element and is adapted to show where to engage the first fastener element with the second fastener element. The visual indicator is adapted to wear upon repeated connection and disconnection of the first and second fastener elements so that the visual indicator fades over time.

[0006] In another aspect, a compression apparatus for applying cyclical compression to an appendage of the body for use in deep vein thrombosis prophylaxis generally comprises an inflatable bladder for being at least partially wrapped around the appendage. A controller is adapted for fluid connection to the bladder for cyclically inflating and deflating the bladder to selectively apply and remove compression from the appendage. Hook material includes a multiplicity of hooks. Loop material includes a multiplicity of loops having a first color and defining a colored hook-engagement area. The loops are engagable by the hooks of the hook material and the loop material to selectively apply and remove compression from the appendage by use in holding the inflatable bladder on the appendage. The loop material further includes another area separate from the hook-engagement area. The loops in the other area have a second color different from the first. The loops of the loop material have the first color adapted to be broken by repeated connection and disconnection of the hook material with the loop material so that the first color of the hook-engagement area becomes less distinct from the second color.

[0007] Compression apparatus for applying cyclical compression to an appendage of the body for use in deep vein thrombosis prophylaxis, the compression apparatus comprising:

an inflatable bladder for being at least partially wrapped around the appendage;

a controller adapted for fluid connection to the bladder for cyclically inflating and deflating the bladder to selectively apply and remove compression from the appendage;

hook material including a multiplicity of hooks;

loop material including a multiplicity of loops having a first color and defining a colored hook-engagement area, the loops being engagable by the hooks of the hook material when the inflatable bladder is wrapped at least partially around the appendage for use in holding the inflatable bladder on the appendage, the loop material further including an other area separate from the hook-engagement area, the loops in the other area having a second color different from the first, the loops of the loop material having the first color being adapted to be broken by repeated connection and disconnection of the hook material with the loop material so that the first color of the hook-engagement area becomes less distinct from the second color;

[0008] A compression apparatus wherein the hook-engagement area comprises a portion less than all of a total surface area of the second fastener element.
A compression apparatus wherein the hook-engagement area is generally oblong in shape.

A compression apparatus comprising plural, spaced apart patches of hook material, and further comprising plural hook-engagement areas spaced apart from each other.

A compression apparatus further comprising hook indicia generally overlying respective ones of the patches of hook material.

A compression apparatus wherein the pressure applicator comprises an inflatable bladder sized and shaped to be at least partially wrapped around the appendage.

A compression apparatus as set forth in claim 10 wherein the loop material has perforations therein.

In yet another aspect, a method of making a compression device for use in applying compression to a part of a wearer's body generally comprises providing a pressure applicator to apply a compression to the wearer's body part when the device is placed on the wearer's body part. Hook material is attached to the device. Loop material is colored in an area selected for attachment of the hook material to the loop material so that the coloring becomes less visible as the loop material and hook material are repeatedly connected and disconnected. The loop material is attached to the device in a location for selective engagement with the hook material for use in securing the compression device to the wearer's body part.

Other features will be in part apparent and in part pointed out hereinafter.

**BRIEF DESCRIPTION OF THE DRAWINGS**

Fig. 1 is a front elevation of a compression sleeve;

Fig. 2 is an exploded perspective of the compression sleeve;

Fig. 3 is a rear elevation of an inner layer of the compression sleeve;

Fig. 4 is a front elevation of an inner layer of the compression sleeve with the outer cover removed;

Fig. 5 is a longitudinal section of the compression sleeve with inflatable bladders of the sleeve in an inflated state;

Fig. 6 is a longitudinal section of the compression sleeve with inflatable bladder in a deflated state;

Fig. 7 is an enlarged fragmentary elevation of the outer cover illustrating loop material;

Fig. 8 is similar to Fig. 1 showing faded hook-engagement areas; and

Fig. 9 is an enlarged, fragmentary front elevation of the compression sleeve with distal flaps secured to an outer face of the sleeve.

Corresponding reference characters indicate corresponding parts throughout the drawings.

**DETAILED DESCRIPTION OF THE DRAWINGS**

Referring now to the drawings, and in particular to Figs. 1 and 2, one embodiment of a compression device (broadly, "a garment or a sleeve") is generally indicated at 10 for applying sequential compression therapy to a limb of a wearer. The compression sleeve is of the type sized and shaped for being disposed around a leg of the wearer, but could be configured for application to other parts, including particularly appendages, of the wearer's body. More specifically, the sleeve 10 has a width W (Fig. 1) for being wrapped around a full circumference of the leg and a length L (Fig. 1) for running from the ankle to a thigh of the leg. It will be understood that a compression sleeve may come in different sizes, such as a knee length sleeve (Fig. 8) that extends from the ankle up the calf of the leg. It is understood that other types of compression devices for being disposed about other parts of the wearer's body (e.g., the foot), are within the scope of this invention, such as a wrap around a patient's chest in the treatment of breast cancer.

A numerical study performed by R.D. Kamm, titled "Bioengineering Studies of periodic External Compression as Prophylaxis Against Deep Vein Thrombosis - Part I: Numerical Studies" concluded, among other things, that "the entire length of the veins should be emptied as full and as rapidly as possible." The Kamm study reviews three types of compression, the one of interest is wavelike compression. Wavelike compression is most similar to sequential compression provided by the illustrated embodiments of the present invention. The Kamm Study found wavelike compression is most effective in moving blood for an effective prophylaxis treatment.

Referring to Figs. 1 and 2, the compression sleeve 10 comprises four layers secured together in the illustrated embodiment of the present invention. The scope of the present invention is not limited to four layers. More specifically, the compression sleeve comprises an inner layer, generally indicated at 12, on which a first intermediate layer (broadly, a first bladder layer), generally indicated at 14, is overlaid. A second intermediate layer (broadly, a second bladder layer), generally indicated at 16, overlies the first intermediate layer 14 and is secured thereto. An outer cover generally indicated at 18, overlies and is secured to the second intermediate layer 16. In use, the inner layer 12 is disposed most adjacent to the limb of the wearer and is in contact with the limb of the wearer, and the outer cover 18 is most distant from the limb of the wearer. A knee opening 19 is formed through the sleeve 10 that is generally aligned with the back of the knee when the sleeve is applied to the leg. The layers have the same geometric shape and are superposed on each other so that edges of the layers generally coincide. It is contemplated that one or more of the layers 12, 14, 16, or 18 may not be superposed on a corresponding layer, but slightly offset to accommodate a particular feature of a patient's limb. Moreover, the number of sheets or thickness making up each layer 12,
14, 16, or 18 of the compression sleeve 10 may be other than described. The thickness of the layers may vary to add strength or to cause more expansion in one direction, such toward the limb, during inflation.

[0029] Referring to Figs. 1, 2 and 4, the first and second intermediate layers 14, 16, respectively, each include a single sheet of elastic material (broadly, "bladder material"). For example, the sheets 14 and 16 are made of a pliable PVC material as the bladder material. Layers 12 and 18 are made of a polyester material. The second intermediate layer 16 is secured to the first intermediate layer 14 via three separate bladder seam lines 22a, 22b, 22c defining a proximal bladder 24a, an intermediate bladder 24b and a distal bladder 24c, respectively, that are spaced apart longitudinally along the sleeve 10. The number of bladders may be other than three without departing from the scope of the present invention. As used herein, the terms "proximal", "distal", and "intermediate" represent relative locations of components, parts and the like of the compression sleeve when the sleeve is secured to the wearer's limb. As such, a "proximal" component or the like is disposed most adjacent to a point of attachment of the wearer's limb to the wearer's torso, a "distal" component is disposed most distant from the point of attachment, and an "intermediate" component is disposed generally anywhere between the proximal and distal components.

[0030] For reasons discussed below, the proximal bladder 24a defines a proximal, lateral extension 25 near the upper edge margin of the sleeve 10. The bladders 24a, 24b, 24c are circumferential bladders meaning that they are sized and shaped to be wrapped around substantially the entire circumference of the wearer's limb or very nearly the entire circumference of the limb. For example, in one embodiment the bladders 24a, 24b, 24c each extend around at least 90% of a median circumference of a leg. However, prior art devices have partial bladders such as AirCast® and HillRom®, and these prior art devices do not provide for openings, elasticity and other features of the present invention. It is to be understood that the construction described herein can be adopted by the prior art sleeves with a partial bladder construction, without departing from the scope of the present invention.

[0031] The intermediate layers 14, 16 may be secured together by radiofrequency welding, adhesive, or other chemical and/or mechanical process. It is understood that the intermediate layers 14, 16 may be secured together at other locations, such as around their peripheries and at bladder seam lines 22a, 22b, 22c to further define the shape of the inflatable bladders 24a, 24b, 24c. For purposes discussed below, the first intermediate layer 14 is secured to the inner layer 12 along a seam line 25 (Figs. 5 and 6) that runs along the outer periphery of the first intermediate layer 14 so that central regions of the bladders 24a, 24b, 24c are not secured to the inner layer 12. This permits the bladders 24a, 24b, 24c to move relative to the inner layer 12. The second intermediate layer 16 may also be secured to the inner layer 12 along the same seam line 25. The first intermediate layer 14 may be secured to the inner layer 12 by RF welding or adhesive or in other suitable ways. This structure improves comfort as described below.

[0032] Referring to Figs. 2 and 4, each inflatable bladder 24a, 24b, 24c receives fluid from a source of compressed fluid (not shown) via a dedicated proximal bladder tube 26a, intermediate bladder tube 26b, and distal bladder tube 26c, respectively. (Fig. 2). A tube line need not be dedicated to a bladder to practice the invention. Each tube 26a, 26b, 26c is disposed between the intermediate layers 14, 16 and secured to the respective bladder 24a, 24b, 24c by the respective bladder seam line 22a, 22b, 22c. As shown best in Figs. 2 and 4, the first intermediate layer 16 defines a cutout 27 (Fig. 2) so that portions of the tubes 26a, 26b, 26c are not disposed between the intermediate layers. Other ways of securing the tubes 26a, 26b, and 26c to the bladders 24a, 24b, and 24c are within the scope of the invention. The opposite ends of the tubes 26a, 26b, 26c are grouped together using a second connector 30 (Figs. 1 and 2) that is adapted to fluidly connect the tubes to the source of compressed fluid. The source of compressed fluid may be an air compressor under the control of a microprocessor that sequentially pressurizes the bladders as is generally known in the art. An exemplary air compressor is described in U.S. Patent No. 5,876,359 to Bock, the disclosure of which is incorporated herein by reference. The bladders 24a, 24b, 24c may be configured to contain air pressurized to at least about 10 mm Hg (1333 Pa) to about 45 mm Hg (6000 Pa). The bladders should be capable of being repeatedly pressurized without failure. Materials suitable for the sheets include, but are not limited to, flexible PVC material that will not stretch substantially. In another embodiment, the intermediate layers may form a chamber for receiving an inflatable bladder that is formed separate from the chamber. In this embodiment, the layers may not be capable of containing pressurized air as long as the inflatable bladders are so capable. It will be noted that the bladders 24a, 24b, 24c can have openings 32 extending completely through the bladders, as described in the embodiments of the present invention.

[0033] Referring particularly to Figs. 1 and 4, the sleeve 10 defines a connecting section including a pair of bridge members 84 on opposite sides of the knee opening 19 that extend between and connect a proximal portion of the sleeve that includes the proximal bladder 24a to the remainder of the sleeve. The proximal tube 26a generally lies along an axis of bridge member 84 to provide structural, lengthwise support to the sleeve 10. As shown best in Fig. 4, the cutout 27 in the intermediate sheet 16 does not extend through the bridge member 84. The proximal tube 26a extends between spaced apart distal spot welds 86 disposed adjacent to a distal end of the bridge member 84 and between spaced apart proximal spot welds 88 disposed adjacent to a proximal end...
of the bridge member. The spot welds secure the tube 26a to the bridge member 84 such that the proximal bladder tube 26a constitutes a rigid structural component (broadly, a “first rigid structural component”) for maintaining the spacing between the proximal bladder 24a and the intermediate bladder 24b and in maintaining the longitudinally structural integrity of the connecting section. In other words, the sleeve 10 is rigidified against collapsing or sliding down the wearer’s leg. As explained above, the proximal bladder tube 26a is secured to the proximal bladder 24a at the proximal, lateral extension 25. The proximal bladder tube 26a runs along a side of a distal portion of the proximal bladder 24a so that it does not enter the bladder until it reaches the proximal, lateral extension 25. Being secured at the proximal, lateral extension 25 of the bladder 24a provides additional longitudinal support to the sleeve 10 because the proximal bladder tube 26a extends lengthwise across more of the proximal portion of the sleeve than if the tube was secured at a distal portion of the bladder. In one embodiment, the proximal bladder tube 26a extends at least a quarter of the way across a thigh section of the sleeve 10. In another embodiment shown in Fig. 4, the tube 26a extends more than half way across the thigh section. This helps to keep the proximal portion of the sleeve 10 from collapsing and/or sliding out of position down the wearer’s leg.

[0034] Referring to Figs. 2 and 4, in addition to the proximal bladder tube 26a, a second rigid structural component 90, disposed between the intermediate layers 14, 16 and extending within the other bridge member 84 of the connecting section, also provides longitudinal structural support to the sleeve 10. The second structural component 90 extends between proximal and distal ends of the bridge member 84. The respective proximal and distal ends of the structural component 90 are wider than an intermediate portion of the component and the periphery of the component generally conforms to the peripheries of side walls of the bridge member 84 so that the structural component is secured to the bridge member.

[0035] Referring to Figs. 3 and 4, the proximal bladder 24a is secured to the inner layer 12 and the outer cover 18 at spot welds 92 adjacent to the bladder openings 32 and within an outer perimeter of the bladder defined by the bladder seamline 22a. The spot welds 92 maintain the outer cover 18 and the inner layer 12 in proper position with respect to the bladders 24a, 24b, 24c. In other words, the spot welds 92 prevent the bladders 24a, 24b, 24c from substantially shifting relative to the inner layer 12 and the outer cover 18 while still providing the sleeve 10 with substantial flexibility. Too much movement of inner layer 12 and the outer cover 18 with respect to the bladders 24a, 24b, 24c may reduce the fit of the sleeve, thereby leading to reduced efficacy of the compression therapy. The proximal bladder 24a is free from securement to the inner layer 12 and outer cover 18 other than at the spot welds 92 to maintain flexibility of the sleeve so that mobility of the patient’s leg is not compromised. Inner layer 12 may be joined to layer 16 at the spot welds 86, 88, 92 or the inner layer 12 may be joined at the seam line 34 of the opening 32. Away from the openings 32 and spot welds 86, 88, 92, the inner layer 12 is not joined to surface of the bladder material forming the bladder that expands to provide compression treatment to the patient’s limb.

[0036] In one embodiment, the bladders 24a, 24b, 24c are constructed to expand more toward the wearer than away from the wearer, thereby applying a greater compressive force on the wearer’s limb. In one example, the first intermediate layer 14 (i.e., the layer most adjacent to the inner layer 12) has a lesser thickness than that of the second intermediate layer 16. With both layers 14, 16 being of the same material (i.e., elastic PVC material) the first intermediate sheet will have a lower modulus of elasticity. Thus, when air is introduced into the bladders 24a, 24b, 24c, the bladders will expand more toward the inner layer 12 and the wearer than away from the wearer. It is understood that other ways, besides a difference in thickness between the intermediate layers 14, 16, of constructing the bladders 24a, 24b, 24c so that they expand more toward the wearer than away from the wearer is within the scope of the invention.

[0037] Referring to Figs. 2 and 3, the inner layer 12 is constructed of a material that is capable of wicking moisture near a patient’s limb. It is understood that the inner liner 12 may be of other configurations, may have other characteristics and properties, and may be formed from other material than described below. The inner (or “wicking”) layer 12, through capillary action, absorbs moisture trapped near the leg or limb of the wearer, carries the moisture away from the surface of the limb, and transports the moisture from locations on the limb at the inner layer 12 where the moisture is abundant to areas where it is less abundant, at the openings 32, for evaporation to the ambient environment. The openings may be of various sizes, shapes and locations within the bladder area providing the compression. An opening 32 exposes the wicking layer to the ambient or surrounding air as opposed to the portion of the wicking layer beneath the bladder material. The portions of the inner layer 12 in registration with the openings 32 may be referred to as “exposed portions”. Other ways of exposing the wicking material are within the scope of this invention, such as slits or extending the wicking material outside the perimeter of the bladder material. The present invention has its exposed portion within the bladder area that provides compression. The compression region is the bladder area expanding and contracting under the influence of air pressure or other fluids. The area of the bladder not providing compression is the seamline or weld points which are points of the bladder material sealed together to provide an air or water tight boundary or other regions of the opposed sheets 14, 16 outside the perimeter of the bladder. The wicking material 12 may be inter-weaved with the impervious material to form the inner layer 12. The wicking material 12 transports moisture to an area of less
moisture. The openings 32 must be engineered to maintain blood velocity, while maximizing evaporation of moisture. Suitable wicking materials may be comprised of, for example, some form of polyester, although they may be comprised of polypropylene. Microfibers may be used. Suitable microfiber materials include, but are not limited to, CoolDry model number CD9604, sold by Quanzhou Fulian Warp Knitting Industrial Co., Ltd., Quanzhou City, Fujian Province, China and CoolMax®, sold by E. I. du Pont de Nemours and Company, Wilmington, Delaware.

For the preferred embodiment, the opening shape is generally shaped like a waterdrop. Each opening 32 is tapered from a first round end portion toward a second, smaller round end portion. The openings 32 may be of other shapes, such as circles, ovals, and slits, without departing from the scope of the invention. The opening shapes may be inter-mixed at the bladder without departing from the scope of the invention.

With respect to each bladder 24a, 24b, 24c, the openings 32 are arranged in a distal row 36 and a proximal row 38 (Fig. 4). Both rows 36, 38 extend across the respective bladder 24a, 24b, 24c along the width W of the sleeve 10. As depicted in the drawings, the openings 32 in each proximal row 38 are inverted medium waterdrop-shaped openings in that the openings taper distally, while the openings in each distal row 36 are right-side-up in that the openings taper proximally. The openings 32 in each distal row 36 are offset along the width W of the sleeve from the openings in the respective proximal row 38. Offsetting the openings 32 distributes the openings evenly across the surface area of the bladders 24a, 24b, 24c, thereby increasing the breathability of the bladders and the overall breathability of the sleeve 10 without compromising the structural integrity of the bladders or their ability to apply compressive force (i.e., prophylaxis treatment) to the leg or body part. Moreover, offsetting the openings in the respective distal and proximal rows 36, 38, also makes the bladders 34a, 34b, 34c more stretchable in the widthwise direction of the sleeve 10. Other ways of allowing fluid wicked by the inner layer 12 to evaporate, besides the openings 32 through the bladders are within the scope of the invention.

Referring to Figs. 1 and 2, the outer cover 18 of the compression sleeve 10 is constructed of a single sheet of material. The outer cover 18 is breathable and has a multiplicity of openings 40 or perforations so that it has a mesh construction to provide even more breathability. It is understood that the outer cover 18 may be of other configurations, may have other characteristics and properties, and may be formed from other material than described below. A suitable material for the outer cover 18 may be a polyester mesh. The rate of evaporation from the openings is improved by treating the fibers of the mesh material with a hydrophilic material. The mesh material will absorb the wicked fluid more readily. Wicking fibers of this type are indicated generally at 21 in Fig. 7. These hydrophilic fibers lower the surface tension of the mesh material to allow bodily fluids to more easily absorb into the fibers and spread therethrough for a more efficient evaporation of the wicked fluid. Absorbing fluid more readily will allow the fluid to move to the open areas more quickly for evaporation. The capillary effect is made more efficient as the absorbed fluid at the openings is moved more quickly through the mesh outer cover 18.

Referring to Figs. 1 and 7, the entirety of an outer surface of the outer cover 18 also acts as a fastening component of a fastening system for securing the sleeve 10 to the limb of the wearer. In a particular embodiment, the outer cover 18 of mesh (Fig. 7), for example, has an outer surface comprising loops 44 (Fig. 7) that acts as a loop component of a hook-and-loop fastening system. A mesh construction, as shown in Fig. 7, has interconnected or weaved fibers 21 of material forming the outer cover 18. The loops 44 may be formed as part of the material of the outer cover 18 or otherwise disposed on the surface of the outer cover. A suitable material with such construction is a polyester mesh loop 2103 sold by Quanzhou Fulian Warp Knitting Industrial Co., Ltd. of Quanzhou City, China. Hook components 46 (Fig. 3) are attached to an inner surface of the inner layer 12 at the proximal, intermediate and distal flaps 41a, 41b, 41c, respectively. The loops 44 of the outer cover 18 allow the hook components 46 (Fig. 3) to be secured anywhere along the outer surface of the outer cover when
the sleeve 10 is wrapped circumferentially around the limb of the wearer. This allows for sleeve 10 to be of a substantially one-size-fits-all configuration with respect to the circumferences of different wearers’ limbs. Moreover, the outer cover 18 having the loops 44 allows the practitioner to quickly and confidently secure the sleeve 10 to the wearer’s limb without needing to align the fastening components.

[0044] The hook components 46 (broadly, first fastener elements*) can be secured anywhere along the outer surface of the sleeve 10 (e.g., outer cover 18), but colored hook-engagement areas 100 are printed using colorant, such as ink or dye, on an outer surface of the outer cover to indicate to the user where the hook components 46 should be secured. This can to assure the proper alignment of the sleeve 10. In the illustrated embodiment, there are three hook-engagement areas 100 (broadly, visual indicators) indicating where each of the corresponding three hook components 46 should be secured on the outer surface of the outer cover 18. The outer cover 18 is formed of or includes loop material that can be broadly considered a second fastening element. Each hook-engagement area 100 comprises a selected area of loops that are of a different color (e.g., blue) than a color of loops (e.g., white) in an adjacent area of the outer surface of the outer cover 18. Each hook-engagement area 100 is also of a different color than the outer surface of the outer cover below the loops. In the illustrated embodiment, each hook-engagement area 100 is a generally oblong or racetrack-shaped area that extends generally transversely with respect to the longitudinal axis of the sleeve 10 generally along the centerlines of each of the three bladder sections of the sleeve 10. However, other colors, shapes and arrangements of a hook-engagement area do not depart from the scope of the present invention.

[0045] Hook indicia 104 is printed on the outer surface of the outer cover 18 to indicate to the user the location of the hook component 46 on the inner face of the sleeve. In the illustrated embodiment, the hook indicia 104 comprise three colored (e.g., blue) hook areas overlying respective ones of the three male fastening components 46. The three colored hook areas are of a different color than the remainder of the outer face lying outside the hook-engagement area 100, and in one embodiment, the hook indicia are the same color as the hook-engagement area. Each of the hook indicia 104 are generally in the shape of a semi-circle. Referring to Fig. 9, upon wrapping the sleeve 10 around the leg and fastening the hook components 46 at the respective hook-engagement areas 100, each hook indicia and corresponding hook-engagement area together form a combined shape that is either oblong or racetrack-shape, or a circle. By forming a shape through connection of the hook component 46 in the hook engagement area 100 that is essentially the same as the original hook engagement area, the user can be assured that the sleeve 10 has been placed on the leg generally in a conforming, aligned configuration. As can be understood, the size of the combined shape correlates directly to the size of a longitudinal opening formed by the wrapped sleeve 10 so that the user is able to determine a proper fit of the sleeve on the leg of the patient. It is understood that the hook-engagement areas 100 and the hook indicia 104 may have other shapes and colors within the scope of the present invention, including other combined shapes. Moreover, each hook-engagement area 100 may have a different color. It is also understood that a loop component with colored loops may be formed separately from the outer cover and secured to the outer surface of the outer cover using adhesives or in other ways.

[0046] During unfastening of the sleeve 10, i.e., as the hooks of the hook components 46 are pulled apart from the colored loops 21 in the hook-engagement area 100, it is believed that fibers forming the loops are broken and/or colorant (e.g., ink) on the loops is removed. As these fibers are broken and/or the colorant is removed, they expose areas of the outer cover 18 underneath that are not colored or of a different color than the loops (e.g., white). In effect, repeated fastening and unfastening of the hooks and loops 21 break the colored loops in the hook-engagement areas 100 and/or removes colorant from the hook-engagement areas so that overall colors of the hook-engagement areas appear to fade and/or actually fade, as illustrated in Fig. 8. It is believed that although the color of each individual loop is not fading when the loops are broken, it appears that the overall color of the hook-engagement area 100 is fading. It is believed that the color of the loops is actually fading when the colorant is being removed by pulling the hook components 46 apart from the colored loops 21. The faded appearance and/or actual fading correlates to a diminution of the fastening force of the hook and loop fasteners, but more generally, this appearance of fading and/or actual fading indicates to the user that the compression device 10 is nearing the end of its lifecycle and needs to be replaced with a new compression device. It is to be understood that the fading appearance and/or actual fading feature may be used with devices other than the compression device 10.

[0047] It is contemplated that the outer cover 18 may be capable of wicking fluid in addition to being breathable. For example, the outer cover 18 may be constructed of the same material as the inner layer 12 (e.g., Cool dry). In this way, the moisture wicked by the inner layer 12 may be wicked by the outer cover 18 through the openings 32 in the bladders 24a, 24b, 24c. The moisture will then spread out evenly across the outer cover 18 and is able to evaporate more readily than if the outer cover was not formed of a wicking material because a greater surface area of the outer cover, as opposed to the inner layer 12, is exposed to air. Alternatively, the cover can have a wicking material laced in or on top of outer layer.

[0048] The compression sleeve 10 as a whole is more comfortable to wear because of the synergistic relationship of the layers 12, 14, 16, 18. For example, the inner
layer 12 is capable of wicking moisture from the limb and allowing the moisture to evaporate out of the sleeve 10. As stated above, wicking involves transporting moisture away from the limb and moving moisture from locations where it is abundant and transporting it to areas where it is less abundant. Material decreases its wicking rate when the moisture is equally distributed in the wicking material and the wicking material is saturated. However, the breathability of the sleeve 10 allows for the wicked moisture to evaporate. The waterdrop-shaped openings 32 in the bladders 24a, 24b, 24c and the breathable outer cover 18 allow moisture in the inner layer 12 that is adjacent to the openings to evaporate therethrough. Accordingly, as the moisture evaporates, it is transported to the drier portions of the inner layer 12, and the inner layer is able to wick more moisture.

[0049] To improve patient mobility, the sleeve was designed to have an elastic inner layer 12 and outer cover 18. An elastic sleeve improves comfort which increases patient compliance. Refer to Figs. 1-7 for the discussion on elasticity below. An elastic device will conform to a patient’s limb to ensure continuous wicking. A compliant or substantially conforming fit will help ensure the contact of the bladder against a patient’s skin during use. The bladder applies the pressure to move the blood. The elastic outer layer helps reduce number of straps to hold the sleeve in place because the elastic outer layer 18 returns its original shape exerting a slight force against the patient’s limb. This force helps hold the sleeve in place and also allows the practitioner not to over tighten a strap. Some prior art devices use an elastic stocking, such as the T.E.D.® stocking, beneath the compression sleeve. The compression sleeve of at least some embodiments avoids the two step process of first placing the compression stocking on the patient, then placing the sleeve over the stocking. Also sleeves of preferred embodiments of the present invention simplify the job of the nurses because there is no need to order a stocking and sleeve.

[0050] The Applicant devised an elasticity test for determining the amount of stretch around the limb and along the limb. A patient needs to be mobile during treatment. Prior art sleeves can be awkward, stiff and heavy so the user would remove the device, if they needed to move about. The need is to improve elasticity without distorting the openings 32 too much such as becoming elongated or causing an opening to overlie, which reduces its size for evaporation.

[0051] For example, the inner layer 12 is preferably elastically stretchable along the width W of the sleeve 10 so that the inner layer is able to conform circumferentially to the shape of the wearer’s limb. Conforming circumferentially allows the inner layer 12 to remain in close, intimate and continuous contact with the wearer’s limb to ensure that the inner layer is continuously wicking moisture from the limb. The inner layer 12 may also be stretchable the length L. Preferably, the inner layer 12 is elastically stretchable along both the width W and the length L of the sleeve and is more elastically stretchable along the length of the sleeve 10 than along the width. Summarizing the preferred approach, using the test described below, the inner layer 12 may have an average elasticity in the widthwise direction of the sleeve of between about 13 lbs/in (23 N/cm) and about 14 lbs/in (25 N/cm), and in one embodiment has an elasticity of about 13.3 lbs/in (23.3 N/cm). The inner layer 12 may have an average elasticity in the lengthwise direction of the sleeve of between about 0.5 lbs/in (0.9 N/cm) and about 0.7 lbs/in (1.2 N/cm), and in one embodiment has an elasticity of about 0.63 lbs/in (1.10 N/cm). The small openings 20 in the inner layer 12 also allow for the inner layer stretch more.

[0052] The outer cover 18 is also elastically stretchable along the length L of the sleeve 10 or stretchable along both lengthwise and widthwise (circumferentially). Preferably, the outer cover 18 is more elastic longitudinally than widthwise. Although elastically stretchable, the outer cover 18 acts to restrain the amount of expansion of the bladders 24a, 24b, 24c. The outer cover 18 helps to conform the bladder to the limb for helping to evenly apply pressure for moving blood. For example, using the elasticity test described below, the outer cover 18 may have an average elasticity in the widthwise direction of between about 13 lbs/in (23 N/cm) and about 15 lbs/in (26 N/cm), and in one embodiment has an elasticity of about 13.6 lbs/in (23.8 N/cm). The outer cover 18 may have an average elasticity in the longitudinally direction of between about 19 lbs/in (33 N/cm) and about 22 lbs/in (39 N/cm), and in one embodiment an elasticity of about 19.8 lbs/in (34.7 N/cm).

[0053] The compression sleeve 10 as a whole is stretchable longitudinally by way of the longitudinally stretchable inner layer 12, intermediate layers 14, 16 and outer cover 18. Further, the sleeve 10 is slightly stretchable widthwise by way of the abilities of the inner layer 12, intermediate layers 14, 16 and the cover 18 to stretch widthwise. The waterdrop-shaped openings 32 and the fact that the openings are offset widthwise also aid in the widthwise stretching.

[0054] It is common for patients that have undergone surgery to incur swelling of the limbs. The widthwise stretching of the sleeve 10 is more comfortable for patients that experience swelling because the sleeve will stretch, i.e., increase in size circumferentially, as the limb swells. Moreover, elasticity of the sleeve 10 allows the wearer to have more mobility of his or her limb and gives the practitioner a greater degree of freedom when wrapping the sleeve around a wearer’s leg. For example, using the elasticity test described below, the thigh-length sleeve 10, comprising the inner layer 12, the intermediate layers 14, 16 and the outer cover 18 as described above, may have an average elasticity in the widthwise direction of between about 22 lbs/in (39 N/cm) and about 27 lbs/in (47 N/cm), and in one embodiment an elasticity of about 24.3 lbs/in (42.6 N/cm). The compression sleeve 10 may have an average elasticity in the lengthwise direction of between about 17 lbs/in (30 N/cm) and about 22 lbs/in
In another example, using the elasticity test described below, a knee-length sleeve, comprising an inner layer, intermediate layers and outer cover of the same material as the thigh-length sleeve described above, may have an average elasticity in the widthwise direction of between about 22 lbs/in (39 N/cm) and about 27 lbs/in (47 N/cm), and an average elasticity in the lengthwise direction of between about 33 lbs/in (58 N/cm) and about 40 lbs/in (70 N/cm).

The following test (herein referred to as the “elasticity test”) is used to measure the elasticity of the layers 12, 14, 16 and 18 and the sleeve 10, both widthwise and lengthwise. First, structure clamps are secured to the structure (e.g., one of the layers 12, 14, 16, and 18 or the sleeve 10) to be tested. When testing the lengthwise or widthwise elasticity, the structure clamps are secured to top and bottom edges of the structure. When testing the widthwise elasticity, the structure clamps are secured to opposite side edges of the structure. The sleeve sample with the structure clamps secured thereto is placed in a universal tensile testing machine (such as a universal testing machine manufactured by Instron® of Grove City, Pennsylvania) by securing the structure clamps to opposing machine clamps of the machine. The machine should include a microprocessor having a tensile force measurement program used to control the machine and record measurements of force and displacement. Once the structure is secured in the machine, the opposing machine clamps are moved apart to a position that eliminates or minimizes the slack in the structure. This position is the initial position for all subsequent tests. The tensile force measurement program is then executed. The displacement of the sleeve sample as the machine clamps are moved apart should be uniform linear elongation and should not damage the structure. This displacement is set and maintained for each test repetition. The test is repeated 7 times for each layer 12, 14, 16 and 18 and the sleeve 10. Elasticity is calculated as force (lbs) divided by the displacement (in). An average elasticity of the 8 tests is calculated by summing the elasticity calculations for the 8 tests and dividing the sum by 8.

The sleeve in some embodiments is made more comfortable for the wearer by the fact that the inner layer 12 and the outer cover 18 are secured to the respective intermediate layers 14, 16 only adjacent to the outer peripheries of the inner layer and cover whereby the bladders 24a, 24b, 24c are not secured directly to the inner layer and cover. This construction allows for the bladders 24a, 24b, and 24c to move independently of the inner layer 12, and vice versa. Co-assigned U.S. Patent Application Serial Number 11/299,568 disclosing an embodiment directed to reducing chafing of a person’s skin during use is incorporated herein by reference.

Thus, when the sleeve 10 is wrapped circumferentially around the wearer’s limb, the inner layer 12 substantially conforms to the contour or shape of the limb and will remain substantially stationary against the wearer’s limb as the bladders 24a, 24b, 24c inflate and deflate and/or shift positions. The movement of the bladders 24a, 24b, 24c both as they inflate and deflate and shift positions relative to the limb may cause chaffing and other discomfort for the patient if the surface of the bladders continuously rubbed against the limb. However, by being secured only at the outer peripheries of the intermediate layers 14, 16, the inner layer 12 creates a buffer between the bladders 24a, 24b, 24c and the limb that prevents chaffing and other friction against the skin of the limb. The bladders 24a, 24b, 24c may move without causing corresponding movement of the inner layer 12 against the skin.

When introducing elements of the present invention or the preferred embodiment(s) thereof, the articles “a”, “an”, “the” and “said” are intended to mean that there are one or more of the elements. The terms “comprising”, “including” and “having” are intended to be inclusive and mean that there may be additional elements other than the listed elements.

As various changes could be made in the above constructions, products, and methods without departing from the scope of the invention, it is intended that all matter contained in the above description and shown in the accompanying drawings shall be interpreted as illustrative and not in a limiting sense.

Claims

1. Compression apparatus for applying cyclical compression to an appendage of the body for use in deep vein thrombosis prophylaxis, the compression apparatus comprising:

   an inflatable bladder for being at least partially wrapped around the appendage;
   a controller adapted for fluid connection to the bladder for cyclically inflating and deflating the bladder to selectively apply and remove compression from the appendage;
   hook material including a multiplicity of hooks; loop material including a multiplicity of loops having a first color and defining a colored hook-engagement area, the loops being engageable by the hooks of the hook material when the inflatable bladder is wrapped at least partially around the appendage for use in holding the inflatable bladder on the appendage, the loop material further including an other area separate from the hook-engagement area, the loops in the other area having a second color different from the first, the loops of the loop material having the first color being adapted to be broken by repeated connection and disconnection of the hook material with the loop material so that the first color of
the hook-engagement area becomes less distinct from the second color.

2. Compression apparatus as set forth in claim 1 wherein the hook-engagement area comprises a portion less than all of a total surface area of the second fastener element.

3. Compression apparatus as set forth in claim 2 wherein the hook-engagement area is generally oblong in shape.

4. Compression apparatus as set forth in claim 2 comprising plural, spaced apart patches of hook material, and further comprising plural hook-engagement areas spaced apart from each other.

5. Compression apparatus as set forth in claim 4 further comprising hook indicia generally overlying respective ones of the patches of hook material.

6. Compression apparatus as set forth in claim 1 wherein the pressure applicator comprises an inflatable bladder sized and shaped to be at least partially wrapped around the appendage.

7. Compression apparatus as set forth in claim 1 wherein the loop material has perforations therein.
## DOCUMENTS CONSIDERED TO BE RELEVANT

<table>
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<th>Category</th>
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<th>Relevant to claim</th>
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**TECHNICAL FIELDS SEARCHED (IPC)**

A61H
A44B

The present search report has been drawn up for all claims.

Examiner: Knoflacher, Nikolaus

**PLACE OF SEARCH**

The Hague

**DATE OF COMPLETION OF THE SEARCH**

14 January 2010

**CATEGORY OF CITED DOCUMENTS**

T: theory or principle underlying the invention
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