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Matrix for iontophoresis
Matrix für Iontophorese
Matrice pour iontophorese

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References cited:
WO-A-93/25168

PATENT ABSTRACTS OF JAPAN vol. 018, no. 222 (C-1193), 21 April 1994 & JP 06 016535 A (JAPAN TOBACCO INC;OTHERS: 01), 25 January 1994,
BACKGROUND OF THE INVENTION

[0001] This invention relates to a dissolution liquid for a drug in iontophoresis which is useful for dissolving a drug in an interface (a skin contactor or patch) for iontophoresis and delivering the drug transdermally, and a method for promoting transdermal or percutaneous absorption of the drug with the use of the dissolution liquid.

[0002] Iontophoresis is a system for promoting or accelerating transdermal absorption (endermic absorption) with the use of electricity as an external stimulus. The principle of such iontophoresis basically resides in promoting or enhancing transmittance of a drug molecule through a skin barrier due to an electric field between an anode and a cathode which is produced by an electric current moving force of a positively charged molecule from the anode to the cathode, and a moving force of a negatively charged molecule from the cathode to the anode [see Journal of Controlled Release, 18, 213-220 (1992); Advanced Drug Delivery Review, 9, 119 (1992); and Pharmaceutical Research, 3, 318-326 (1986)].

[0003] Recent advances of synthetic technologies and genetic engineering insure pure and mass production of a naturally-occuring peptide or protein, or a peptide or protein in which the amino acid composition of the naturally-occuring peptide or protein is changed, or a chemically-modified derivative thereof. Therefore, an application of these peptides or proteins as drugs (medicaments) has been desired. On the other hand, it has been recognized that various physiological activities are physiologically controlled by delicate and complicated in vivo kinetics with advanced researches for these peptides or proteins. Therefore, a system capable to a strict control of the administration (dosage) of these peptides or proteins is required to achieve the maximum drug effects in a specific disease and minimizing side effects (adverse reaction).

[0004] By way of illustration, calcitonin inhibits (suppresses) the decrease of the amount of the bone by inhibiting the bone resorption. Hence, calcitonin is used for treatment (therapy) of osteoporosis, Paget's disease or other diseases. Although an excessive administration of the calcitonin causes a side effect such as anorexia (inappetence), frequent administration (frequent dosage), that is, repeated administration of the calcitonin is required for promoting therapeutic effects for the disease. Further, some peptides exhibit different drug effects depending on a medication process. Taking parathyroid hormone as an example, it has been known that the parathyroid hormone has incompatible effects or activities of deosification activity and ossification promoting activity, and the deosification activity is strongly exhibited when the hormone is administered by intravenous injection at a slow rate, and ossification promoting activity is clearly expressed when the hormone is administered by frequent hypodermic injections. Accordingly, when the parathyroid hormone is used as a therapeutical drug for osteoporosis in expectation of its ossification activity, a pharmaceutical preparation comprising the hormone should be not a sustained releasable preparation but a pulse-releasable preparation.

[0005] However, such physiologically active peptide or protein is generally decomposed by a digestive fluid or juice in a gastrointestinal tract (digestive tract) or hydrolyzed by a hydrolase present in the digestive tract wall, and hence absorption efficiency of the peptide or protein can hardly be improved effectively. Therefore, sufficient drug effect of such physiologically active peptide or protein is not expected by oral administration, and it is usually administered by an injection. Administration as an injectable preparation, however, causes a great pain to a patient and burdens him with a heavy load since such injectable preparation can not be administered by himself. Still more, when repeated and continuous administration is required such as in the calcitonin or parathyroid hormone, the pain and burden of the patient are increased, particularly speaking.

[0006] In the field of pharmaceutical preparations, the iontophoresis is intensively researched as a new drug delivery system capable of corresponding to administration or delivery of such physiologically active peptide or protein. That is, development of a pharmaceutical preparation comprising a drug hitherto administrable only as an injection and being administrable by a patient himself with the use of the iontophoresis will provide a therapy at home. Further, an optional absorption pattern of a drug can be constructed by means of an precise control of an electric voltage or current application time (period). In particular, when the iontophoresis is applied supplemental therapy (treatment) of an endogenous compound in consideration of circadian rhythm of a living body, more effective therapy with it is expected to be realized.

[0007] In a drug delivery system (administration system) with the use of the iontophoresis having such advantages, an electrode for application of an electric current, a membrane holding or supporting a drug (an interface as a skin contactor or patch) which is conductible to the electrode and capable of making contact with a skin, and a reference electrode are generally employed. The drug supported by the drug-supporting membrane is dissolved with a drug dissolution liquid contained in a spacer capable of making contact with the drug-supporting membrane.
[0008] An interface for iontophoresis which comprises a drug-supporting membrane and a spacer containing a drug dissolution liquid is in a small size and has a high drug absorptivity. Use of the above interface, however, moisture content in a surface to be made contact with the skin and in the drug-supporting membrane is decreased due to transpiration or evaporation of the drug dissolution liquid during the application of the electric current, and hence electric conductivity (applicability of electric current) is deteriorated. Hence, the iontophoresis using an interface having such construction does not provide a satisfactorily sufficient transdermal drug delivery (drug absorption) with a prolonged application of the interface. Therefore, suppression of the transpiration of the dissolution liquid seems to ensure maintenance of the electric conductivity over a long period, and to provide sufficient transdermal drug delivery by means of iontophoresis.

[0009] WO-A-93/25168 discloses inhibition of an initial burst of transdermal absorption by using a transdermal absorbent (drug composition) containing a drug and 0.1 to 50% (v/v) of glycerin in a transdermal drug delivery system. This literature describes that the form of the drug composition is gel, cream or others, and the drug composition may comprise an adhesive for supporting the composition in a site to which the composition is applied.

[0010] WO 90/08571 discloses a drug layer of an interface for iontophoresis as produced with the use of a hard porous material or a gel, and water or a polyhydric alcohol such as glycerin as a softening plasticizer.

[0011] WO-A-93/10163 discloses a preparation process of a hydrophilic gel which comprises irradiating an aqueous composition comprising a crosslinkable water-soluble polymer such as a polyethylene oxide, about 1 to 40% by weight of a humectant such as glycerin or propylene glycol, and a crosslinking accelerator with a radiation. This literature also describes an application of the hydrophilic gel to a patch or an electrode assembly. This prior art, however, fails to disclose the use of a polyhydric alcohol or an amino acid for inhibiting moisture in a dissolution liquid in iontophoresis. Further, the use of such drug composition, drug layer or hydrophilic gel for transdermal drug administration by iontophoresis may occasionally result in an increased skin irritation when applying electric current.

SUMMARY OF THE INVENTION

[0012] It is an object of the present invention to provide a drug dissolution liquid which is useful for inhibiting transpiration of moisture from the drug dissolution liquid and hence maintaining electric conductivity (applicability of an electric current) over a long period of time.

[0013] It is another object of the invention to provide a drug dissolution liquid which is advantageous for transdermal drug absorption in terms of high bioavailability and excellent reproducibility.

[0014] A further object of the invention is to provide a drug dissolution liquid which ensures mitigation of skin irritation occurring when applying electric current during iontophoresis.

[0015] It is yet another object of the invention to provide an interface for iontophoresis and a drug delivery system using of the above-mentioned drug dissolution liquid.

[0016] A still further object of the invention is to provide an efficient method for promoting transdermal absorption of a drug which promotes transdermal absorption of a drug held or supported by an interface.

[0017] Therefore, the present invention relates to an interface (6) for iontophoresis comprising a matrix for holding or supporting a drug in a drug dissolution liquid comprising a humectant characterised in that the matrix is a porous matrix.

[0018] In a further embodiment the present invention relates to the use of a humectant in iontophoresis for promoting transdermal absorption of a drug held or supported by an interface (6), wherein the interface comprises porous matrix.

[0019] It was found that incorporation of a humectant into a drug dissolution liquid in an interface for iontophoresis ensures long-term maintenance of conductivity (applicability of an electric current) and provides transdermal administration of a drug with a remarkably high bioavailability and excellent reproducibility.

[0020] Thus, (1) the drug dissolution liquid is a dissolution liquid for transdermal drug delivery by iontophoresis using an interface comprising a porous matrix holding or supporting a drug, which comprises a humectant. The humectant may include at least one member selected from the group consisting of polyhydric alcohols, sugar alcohols, amino acids and acidic mucopolysaccharides. The polyhydric alcohol may, for example, be a polyhydric alcohol having 2 to 4 hydroxyl groups per molecule, such as glycerin. The amino acid may be an amino acid having a nitrogen-containing heterocycle such as a nonaromatic nitrogen-containing 5-membered heterocycle (e.g. proline, hydroxyproline). Typically, the concentration of the humectant may be selected within an adequate range, and the content of the polyhydric alcohol may be 10 to 50% by weight, and the concentration of the amino acid may be 1 to 30% by weight.

[0021] The drug (medicament or medicine) includes physiologically active peptides or proteins, or non-peptide physiologically active compounds.

[0022] The present invention also discloses (2) an interface for iontophoresis which comprises a porous matrix holding or supporting a drug, and a humectant, (3) a transdermal drug delivery (absorption) system which is provided with an interface capable of making contact with a skin and comprising a matrix holding or supporting a drug, a dissolution liquid for dissolving the drug containing a humectant, and a supply means for supplying the dissolution liquid to the skin.
interface for transdermal delivery of the drug dissolved with the dissolution liquid by means of iontophoresis. The matrix in the interface and the system may be a non-gel and porous matrix in the form of a sheet. The humectant may be held or supported at least in an area or region to which an electric current can be applied.

[0023] Further, (4) an applicator is disclosed which comprises an electrode to which an electric voltage can be applied, and an interface being conductible to the electrode, capable of making contact with a skin and holding or supporting a drug. The applicator is capable of being supplied with an aqueous solution containing a humectant for dissolution of the drug.

[0024] The present invention can be used for promoting transdermal absorption of a drug by an interface for iontophoresis which comprises holding or supporting of a drug and a humectant at least in an area to which an electric current is applied.

[0025] It should be understood that the codes with respect to amino acids, peptides and so forth as used in the present specification are based on codes according to IUPAC-IUB Commission on Biochemical Nomenclature, or conventional codes used in the art. When there are optical isomers for an amino acid, the amino acid represents an L-form, unless otherwise specifically defined.

BRIEF DESCRIPTION OF THE DRAWINGS

[0026] Fig. 1 is a cross sectional view illustrating an embodiment of an applicator.
Fig. 2 is a graph showing changes of the concentration of hPTH (1→34) in the serum (sometimes referred to briefly as serum hPTH (1→34) concentration) versus time (time passage) in Example 1, Comparative Example 1 and Comparative Example 2.
Fig. 3 is a graph showing changes of the serum hPTH (1→34) concentration versus time in Example 4 and Comparative Example 2.
Fig. 4 is a graph showing changes of the serum hPTH (1→34) concentration versus time (time passage) in Example 5 and Example 6.

DETAILED DESCRIPTION OF THE INVENTION

[0027] The present invention is now described in detail referring to the drawings if necessary.
[0028] The humectant contained in the drug dissolution liquid is not particularly limited as far as it is a substance which ensures inhibition of transpiration of moisture from the drug dissolution liquid, and provides maintenance or reservation of moisture (water) in the surface to be contacted with the skin and in the drug-supporter (drug-holder) in the interface and which does not adversely affect the skin. The humectant includes, for instance, (1) polyhydric alcohols, (2) sugar alcohols, (3) amino acids and (4) acidic mucopolysaccharides. These humectants may be used singly or in combination.

[0029] The polyhydric alcohol (1) includes, for example, glycerin, ethylene glycol, propylene glycol, 1,3-butylene glycol, pentaerythritol, polyethylene glycol, adducts in which ethylene oxide is added to these polyhydric alcohols (e.g. dioxyethylene glycol, trioxethylene glycol, polyoxyethylene glycol, an ethylene oxide-propylene oxide copolymer, a glycerin-ethylene oxide adduct, a penta-erythritol-ethylene oxide adduct, etc.). Such polyhydric alcohols can be employed independently or in combination. Preferred examples of the polyhydric alcohol include polyhydric alcohols each having 2 to 4 hydroxyl groups per molecule, in particular glycerin.

[0030] As the sugar alcohol (2), there may be mentioned for example xylitol and other pentitol, sorbitol, mannitol, galactitol and other hexitol. These sugar alcohols may also be used singly or in combination.

[0031] Examples of the amino acid (3) include (i) an amino acid constituting a protein, (ii) a naturally-occurring amino acid derived or obtained as a metabolite of a microorganism, or an animal or plant component, and (iii) an amino acid obtained by organic synthesis.

(i) The amino acid constituting the protein includes glycine, alanine, valine, leucine, isoleucine and other aliphatic monoaminononocarboxylic acids; serine, threonine and other aliphatic hydroxyamino acids, aspartic acid, glutamic acid and other acidic amino acids; asparagine, glutamine and other acidic amino acid amides; phenylalanine, tyrosine, tryptophane and other aromatic amino acids; proline, hydroxyproline and other amino acids each having pyrrolidine ring; pyroglutamic acid (pyrrolidone-carboxylic acid) and other amino acids each having pyrrolidine ring; arginine, lysine, histidine and other basic amino acids; methionine, cystine, cysteine and other sulfur-containing amino acids, for instance. The amino acids may be employed independently or in combination.

(ii) As the naturally-occurring amino acid derived or obtained as a metabolite of a microorganism or an animal or plant component, there may be mentioned, for example, L-α-amino butyric acid, γ-amino butyric acid, β-amino-
Examples of (iii) the amino acid obtained by organic synthesis include trimethylglycine, 6-aminohexanoic acid, 8-aminooctanoic acid, 12-aminododecanoic acid and other aliphatic amino carboxylic acids, 4-aminobenzoic acid, 4-(aminomethyl)benzoic acid, 4-(N-(carboxymethyl)aminomethyl)benzoic acid and other aromatic amino carboxylic acids.

The amino acid may be used in the form of a salt. The salt of the amino acid includes, for example, a salt with a base [e.g. ammonia, alkali metals (e.g. sodium, potassium) and other inorganic bases, and trimethylamine, triethylamine and other organic bases], and a salt with an acid [hydrochloric acid, sulfuric acid, phosphoric acid and other inorganic acids, and acetic acid, propionic acid, p-toluenesulfonic acid and other organic acids].

Typically, preferred amino acids include amino acids each having a nitrogen-containing heterocycle (e.g. proline, hydroxyproline and other amino acids having pyrrolidine ring, pyrrolidonecarboxylic acid, histidine, tryptophane and other amino acids constituting a protein) or salts thereof. Among them, amino acids each having a nonaromatic nitrogen-containing 5-membered heterocycle (e.g. amino acids each having pyrrolidine ring such as proline and hydroxyproline and pyrrolidonecarboxylic acid) or salts thereof can advantageously be employed.

The acidic mucopolysaccharide includes, for instance, hyaluronic acid, chondroitin sulfate, and salts thereof [e.g. salts with alkali metals (e.g. sodium, potassium)].

Among these humectants, polyhydric alcohols (in particular glycerin) and amino acids or salts thereof (such as proline and other amino acids each having a nitrogen-containing heterocycle) may preferably be used. The use of the amino acid (in particular, proline and other amino acids each having a nitrogen-containing heterocycle) or its salt ensures remarkable mitigation of skin irritation occurring when applying electric current and provides an increased quantity of applied electricity when applying an electric current subsequent to a first application of current in case that transdermal absorption is conducted in several steps at periodic intervals, and hence ensures an improved transdermal absorptivity.

The content of the humectant in the drug dissolution liquid comprising an aqueous solution may be selected from a suitable range, according to the species of the humectant, which suppresses the transpiration of moisture from the drug dissolution liquid and reserves the moisture on the surface of the skin and in the drug-supporter (drug-holder). The content of the humectant is, for example, 1 to 90% by weight, preferably 1 to 80% by weight, and more preferably 1 to 50% by weight based on the amount of the drug dissolution liquid. Among them, the amino acid and its salt leads to a high retention of moisture even if used in a small amount. More concretely, when the humectant is a polyhydric alcohol such as glycerin, the content of the humectant in the drug dissolution liquid is, for instance, 5 to 50% by weight (e.g. 10 to 50% by weight), and preferably 20 to 40% by weight. When the humectant is the amino acid or its salt, the proportion of the humectant in the drug dissolution liquid is 1 to 30% by weight, preferably 5 to 25% by weight, and more preferably 10 to 20% by weight.

As the drug-support (drug-supporter, drug-holder, matrix) constituting an interface for iontophoresis, a nongel member (hereinafter may simply be referred to as "porous body") may be used which is capable of contacting the skin, holding (retaining) or supporting a drug, which and has a porous or capillary structure through which the drug permeates. Such a porous body includes organic porous bodies (e.g. fibrous aggregates made from cellulose and other naturally-occurring fibers, cellulose acetate and other semisynthetic fibers, polyethylene, polypropylene, nylon, polyester and other synthetic fibers, paper and other sheets, woven or nonwoven and other fabrics, a porous polypropylene, a porous poly(methyl methacrylate), a porous nylon, a porous polysulfone, a porous fluoreoresin and other porous synthetic resins).

The configuration or shape of the porous body is not particularly limited and, for practical purposes, the porous body may be in the form of a sheet. The thickness of the sheet-like porous body can be selected depending on the amount of the drug to be retained (held) and is for example 1 to 500 µm, and preferably 10 to 200 µm. The porous body may be a deformable body, but it may practically have flexibility.

The area of the sheet-like porous body may suitably be selected from a range depending on the holding amount of the drug, and is 1 to 10 cm² and preferably 2 to 8 cm².
The pore size of the sheet-like porous body may be selected within a range not interfering with the holding amount and releasability of the drug. The mean pore size is, for example, 0.01 to 20 µm, preferably 0.1 to 20 µm (e.g. 0.2 to 20 µm) and most preferably 1 to 10 µm.

During the application of the interface comprising a non-gel porous body holding or supporting a drug to a surface contacting the skin, the drug can be absorbed transdermally in a manner which is highly effective and reproducible high effectiveness through the matrix (porous body) by dissolving the drug in the drug dissolution liquid.

The drug to be administered through the interface is not particularly limited as long as it is absorbed transdermally or percutaneously and water-soluble, and various physiologically active peptides or proteins or nucleic acids, or non-peptide physiologically active compounds of a low molecular weight can be employed. The molecular weight of the physiologically active peptide or protein or nucleic acid is, for instance, 100 to 30,000, preferably 200 to 20,000, more preferably 500 to 10,000 and most preferably 500 to 8,000). The molecular weight of the non-peptide physiologically active compound with a low molecular weight is not greater than 1,000 (e.g. 100 to 1,000).

As the physiologically active peptide, there may be mentioned, for example, the following peptides: Luteinizing hormone-releasing hormone (LH-RH), derivatives each having a similar function or activity to LH-RH, such as nafarelin and a polypeptide shown by the following formula (I):

\[(\text{Pyr}) \text{Glu-R}^1 \text{-Trp-Ser-R}^2 \text{-R}^3 \text{-R}^4 \text{-Arg-Pro-R}^5\]  

wherein R^1 represents His, Tyr, Trp or p-NH_2-Phe, R^2 represents Tyr or Phe, R^3 indicates Gly or a D-amino acid residue, R^4 denotes Leu, Ile or Nle, R^5 represents Gly-NH-R^6, where R^6 denotes a hydrogen atom or a lower alkyl group which may have a hydroxy group, or NH-R^6, where R^6 has the same meaning as above, or a salt thereof [see U.S. - A - 3853837, U.S. - A - 4008209, U.S. - A - 3972859, GB-A-1423083, Proceedings of the National Academy of Science, 78, 6509-6512 (1981)].

As examples of the D-amino acid residue shown by R^2 in the formula (I), there may be mentioned α-D-amino acid having 9 carbon atoms or less (e.g. D-Leu, Ile, Nle, Val, Nval, Abu, Phe, Phg, Ser, Thr, Met, Ala, Trp, α-Aibu). These amino acids may have a protective group (e.g. t-butyl, t-butoxy or t-butoxycarbonyl group). The lower alkyl group shown by R^6 includes, for example, alkyl groups each having 1 to 6 carbon atoms (e.g. methyl, ethyl, propyl, isopropyl, butyl and t-butyl groups).

A salt (e.g. a salt with an acid) or metallic complex compound of the peptide shown by the formula (I) can also be used in the similar manner as the peptide of the formula (I).

Among the polypeptides shown by the formula (I) a polypeptide (TAP-144) wherein R^1 = His, R^2 = Tyr, R^3 = D-Leu, R^4 = Leu and R^5 = NHCH_2-CH_3 is preferably employed.

LH-RH antagonists such as a polypeptide shown by the following formula (II):

\[N-\alpha-t-butoxycarbonyl-O-benzyl-Ser-Trp-Ser-Tyr-X_1-Leu-\text{Arg-Pro-GlyNH}_2\]  

wherein X_1 represents D-Ser or D-Trp, or a salt thereof [see U.S. - A - 4086219, 4124577, 4253997, and 4317815].

Snake poison (venom) peptides each having antagonistic activity against GPIIb/IIIa, such as barbourin, peptides having Arg-Gly-Asp sequence, such as Arg-Gly-Asp-Ser, Gly-Arg-Gly-Asp-Ser-Pro, SK&F-106760 (cyclo-S, S-[Ac-Cys(Nα-methyl)Arg-Gly-D-Asp-penicillamine]-NH_2), and other peptide-like compounds having a similar function or activity, such as (S)-4-[(4-aminobenzoyl)glycyl]-3-methoxy-carbonylmethyl-2-oxopiperazine-1-acetic acid, (S)-4-(4-guanidinobenzoyleamino)acetyl-3-[3-(4-guanidinobenzoyleamino)propyl-2-oxopiperazine-1-acetic acid hydrochloride, MK-383 (2-S-(n-butylsulfonyl)amino)-3-[4-(N-piperidin-4-yl)butyloxyphenyl)-propionic acid·HCl), L-70462 (L-Tyr-N-(butylsulfonyl)-O-[4-(piperidinyl)butyl] mono-hydrochloride), SC-5684 (ethyl [(4-(aminomimethyl)phenyl) amino]-1,4-dioxo-butyl]amino-4-pentinoate), Ro-44-9883 ([1]-N-(p-amidinophenyl)-L-Tyr-4-piperidinyl) jacetic acid), DMP728 (cyclic [D-2-aminoethyl-N-2-methyl-L-Arg-Gly-L-Asp-3-aminomethyl-benzoic acid] methanesulfonate).

Insulin; somatostatin, somatostatin derivatives, such as a polypeptide shown by the following formula (III):
wherein Y represents D-Ala, D-Ser or D-Val, Z represents Asn or Ala, or a salt thereof [see U.S. -A-4087390, 4093574, 4100117 and 4253998], growth hormone, growth hormone-releasing hormone; prolactin; adrenocorticotropic hormone (ACTH); melanocyte-stimulating hormone (MSH); thyroid stimulating hormone-releasing hormone (TRH), and derivatives thereof, such as a compound shown by the following formula (IV):

wherein $X^a$ represents a 4- to 6-membered heterocyclic group, $Y^a$ denotes imidazol-4-yl or 4-hydroxylphenyl group, $Z^a$ represents CH$_2$ or S, $R^{1a}$ and $R^{2a}$ independently represent a hydrogen atom or a lower alkyl group, and $R^{3a}$ represents a hydrogen atom or an optionally substituted aralkyl group, or a salt thereof [see Japanese Patent Application Laid-open No. 121273/1975 (JP-A-50-121273), Japanese Patent Application Laid-open No. 116465/1977 (JP-A-52-116465)].

[0050] Thyroid stimulating hormone (TSH); luteinizing hormone (LH); follicle-stimulating hormone (FSH); parathyroid hormone (PTH), derivatives each having a similar function or activity to the parathyroid hormone, such as a peptide shown by the following formula (V):

wherein $R^{1b}$ represents Ser or Aib, $R^{2b}$ represents Met or a naturally-occurring fat-soluble amino acid, $R^{3b}$ denotes Leu, Ser, Lys or an aromatic amino acid, $R^{4b}$ represents Gly or a D-amino acid, $R^{5b}$ denotes Lys or Leu, $R^{6b}$ represents Met or a naturally-occurring fat-soluble amino acid, $R^{7b}$ denotes Glu or a basic amino acid, $R^{8b}$ represents Val or a basic amino acid, $R^{9b}$ represents Trp or 2-(1,3-dithiolan-2-yl)Tyr, $R^{10b}$ denotes Arg or His, $R^{11b}$ represents Lys or His, $R^{12b}$ represents Lys, Gln or Leu, and $R^{13b}$ represents Phe or Phe-NH$_2$, or a salt thereof [see Japanese Patent Application Laid-open No. 32696/1993 (JP-A-5-32696), Japanese Patent Application Laid-open No. 247034/1992 (JP-A-4-247034), EP-A-510662, EP-A-77885, EP-A-539491], a peptide fragment of the N-terminus (1→34-position) of a human PTH (hereinafter referred to as hPTH (1→34) [G.W. Tregear et al., Endocrinology, 93, 1349-1353 (1973)]; vasopressin, vasopressin derivatives [desmopressin [see Journal of Society of Endocrinology, Japan, 54, No. 5, 676-691 (1978)]].

[0051] Oxytocin; calcitonin, derivatives each having a similar function to calcitonin, such as a compound shown by the following formula (VI):

wherein $X^b$ represents D-Ala, D-Ser or D-Val, $Y^b$ denotes Leu, Lys, Ser-Glu-Leu-Gly-Leu-Leu-Ser-Gln-Glu-Leu-His-Lys-Leu-Gln-Thr-Tyr-Pro-Arg-Thr-Asp-Val-Gly-Ala-Gly-Thr-Pro (VI)
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wherein X represents 2-aminoseric acid, or a salt thereof [Endocrinology, 1992, 131/6 (2885-2890)]; glucagon; gastrins; secretin; pancreozymin; cholecystokinin; angiotensin; human placental lactogen; human chorionic gonadotropin (HCG).

[0052] Enkephalin, enkephalin derivatives, such as a peptide shown by the following formula (VII):

![Chemical Structure](image)

wherein R1 and R3 denote a hydrogen atom or an alkyl group having 1 to 6 carbon atoms, R2 represents a hydrogen atom or a residue of a D-α-amino acid, R4 denotes a hydrogen atom or an optionally substituted aliphatic acyl group having 1 to 8 carbon atoms, or a salt thereof (see U.S.-A-4229438, European Patent Application Laid-open No. 31567 (EP-A-31567)) and other oligopeptides and endorphins.

[0053] Kyotorphine; interferons (α-, β-, γ-interferons); interleukins (e.g. interleukins I to XII); tuftsin; thymopoietin; thymostimulin; thymus humoral factor (THF); factor of thymus in serum (FTS) and their derivatives, such as a peptide shown by the following formula (VIII):

![Chemical Structure](image)

wherein X represents L- or D-Ala, Y and Z independently represent Gly or a D-amino acid residue having 3 to 9 carbon atoms, or a salt thereof (see U.S.-A-4229438); and other thymus hormones [e.g. thymocin α1 and β4, thymic factor X, etc.].

[0054] Tumor necrosis factor (TNF); colony stimulating factor (CSF); motilin; dynorphin; bombesin; neurotensin; cerulein; bradykinin; urokinase; asparaginase; kallikrein; substance P; nerve growth factor; factor VIII and factor IX of blood coagulation factors; lysozyme chloride; polymyxin B; colistin; gramicidin; bacitracin; protein synthesis-stimulating peptide (GB-A-8232082); gastrin inhibitory polypeptide (GIP); vasoactive intestinal polypeptide (VIP); platelet-derived growth factor (PDGF); growth hormone-releasing factor (GRF, somatoclinine, etc.); born morphogenetic protein (BMP); epithelium growth factor (EGF); preproctostatin (Nature, 381, 242-245 (1996)), erythropoietin.

[0055] These physiologically active peptides may be human peptides, or peptides derived from animals such as bovines, swine, chickens, salmon, eel and so forth. Further, the peptide may be a chimera of a human peptide and a peptide derived from the above animal, or an active derivative in which a part of the structure of the peptide has been changed. By way of an example, the insulin may be an insulin derived from a swine or a chicken, salmon, eel, or a peptide which is a chimera of a human and salmon and is shown by the following formula (IX) [Endocrinology, 1992, 131/6 (2885-2890)]:

![Chemical Structure](image)

wherein X represents L- or D-Ala, Y and Z independently represent Gly or a D-amino acid residue having 3 to 9 carbon atoms, or a salt thereof (see U.S.-A-4229438); and other thymus hormones [e.g. thymocin α1 and β4, thymic factor X, etc.].

[0056] Preferred examples of the drug include physiologically active peptides and their derivatives, such as a calcitonin, adrenocorticotropin hormone, parathyroid hormone (PTH), hPTH (1→34), insulins, secretin, oxytocin, angiotensin, β-endorphin, glucagon, vasopressin, somatostatin, gastrins, luteinizing hormone-releasing hormone, enkephalins, neurotensin, growth hormone, growth hormone-releasing hormone, bradykinin, substance P, dynorphin, thyroid stimulating hormone, prolactin, interferons, interleukins, G-CSF, glutathione peroxidase, superoxide dismutase, desmopressin, somatomedin, endothelin, and their salts. Further, nucleic acids, nucleo-tides and various antigenic proteins may also be employed.

[0057] The salt of the physiologically active peptide or its derivative includes, for instance, a salt with an inorganic acid such as hydrochloric acid, sulfuric acid, hydrobromic acid and phosphoric acid; a salt with an organic acid such
as formic acid, acetic acid, propionic acid, glycolic acid, oxalic acid, succinic acid, tartaric acid, citric acid, benzenesulfonic acid and p-toluenesulfonic acid; a complex salt with an inorganic compound such as calcium and magnesium.

The nonpeptide physiologically active compound includes compounds each having a molecular weight of 1,000 or less and having pharmacological activity. The species of the nonpeptide physiologically active compound is not particularly limited, and as the compound, there may be mentioned for example antibiotics, antymykosis (antifungal drugs), hypolipidermic drugs, circulatory drugs, vasoconstrictors, antiplatelet drugs, antitumor drugs, antipyretic, analgesic and/or antiinflammatory agents, antithrombotic agents, sedatives, muscle relaxants, antiepileptic drugs, antitumor drugs, antidepressants, potentiative-diuretic agents, drugs for diabetes, anticoagulants, hemostatic agents, antituberculosis drugs, hormones, narcotic antagonists, bone resorption-inhibitory agents, osteogenetic promoting agents, angiogenesis inhibitors.

The antibiotic includes, for instance, gentamycin, lividomycin, sisomycin, tetracycline hydrochloride, ampicillin, cefalolin, cefotiam, cefazolin, tienamycin, sulfazecin.

The antifungal includes, for example, 2-[(1R,2R)-2-(2,4-difluorophenyl-2-hydroxy-1-methyl-3-(1H-1,2,4-triazol-1-yl)propyl]-4-[3-(2,2,3,3-tetrafluoropropoxy)phenyl]-3(2H,4H)-1,2,4-triazolone, 1-[(1R,2R)-2-(2-fluorophenyl)-2-hydroxy-1-methyl-3-(1H-1,2,4-triazol-1-yl)propyl]-3-[4-(2,2,3,3-tetrafluoropropoxy)phenyl]-2-imidazolidinone.

Examples of the vasoconstrictors include prostaglandin E2 and prostaglandin F2.

Examples of the antiplatelet drug (antiplatelet drug) include paravastatin and simvastatin. The circulatory drug includes delapril hydrochloride.

As the antiplatelet drug, there may be mentioned, for example, ticlopidine, cilostazol, limaprostat, aspirin.

The antitumor drug (antineoplastic agent) includes, for instance, bleomycin hydrochloride, actinomycin-D, mitomycin-C, adriamycin and fluorouracil.

As examples of the antipyretic, analgesic and/or antiinflammatory agent, there may be mentioned sodium salicylate, subpyrine, indomethacin sodium, hydroxymorphone, morphine hydrochloride, fentanyl, buprenorphine.

The antithrombotic agent includes, for instance, pentolinium, hexamethonium bromide.

As the muscle relaxant are pridinol methanesulfonate, tubocurarine chloride.

Examples of the hormone drug include estradiol, testosterone, prednisolone succinate, dexamethasone.

Examples of the hypolipidermic drug (antihyperlipidermic drug) include paravastatin and simvastatin. The circulatory drug includes delapril hydrochloride.

As the antiepileptic agent, there may be mentioned for instance phenytoin sodium, ethosuximide.

As the sedative, there may be mentioned alphaprodine hydrochloride, and atrerine sulfate, for instance. Examples of the muscle relaxant are pridinol methanesulfonate, tubocurarine chloride.

As the antidepressant, there may be mentioned for instance imipramine and phenelzine sulfate.

The antiulcer drug includes, for example, metoclopramide. As the antidepressant, there may be mentioned for instance imipramine and phenelzine sulfate.

Examples of the antiallergic agent are diphenhydramine hydrochloride, triprolidine hydrochloride, clemizole hydrochloride.

As the cardiotonic, there may be mentioned trans-n-o xo camphor and theophyllol, for example. The antihypertensive agent includes, for instance, propranolol hydrochloride and oxrenolol hydrochloride. Examples of the vasodilator include oxyfedrine hydrochloride, tolbutamide hydrochloride.

The hemostatic includes menadione sodium bisulfite, acetenonaphtone and tranexamic acid, typically speak-

As the antitumor drug, there may be mentioned, for example, cisplatin, ethambutol.

Examples of the anticoagulant include beta-estradiol, testosterone, prednisolone succinate, dexamethasone.

The antitussive/expectorant agent includes, for example, ephedrine hydrochloride, codeine phosphate and picoperidamine hydrochloride.

As the angiogenesis inhibitor, there may be mentioned, for example, a vascularization inhibitory steroid [see Science 221, 719 (1983)], fumagillol derivatives, [e.g. O-monochloroacetyl-carbamoylfumagillol, O-dichloroacetylcarbamoylfumagillol (see EP-A-357061, EP-A-359036, EP-A-4152943)].

The drug may be held or supported by the drug holder (porous body) by dissolving the drug in distilled water for injection, a physiological saline for injection to give an aqueous solution, and applying the solution to the drug holder in a conventional manner such as by impregnation, spraying, application, dropwise-adding and subsequently drying.

When the drug is the physiologically active peptide or protein, a dissacharide (e.g. trehalose, maltose, mannitol and inositol) may be added to the aqueous solution containing the drug in order to improve the stability of the drug in dry conditions. The proportion of the dissacharide is, for example, 0.1 to 10 mg/ml, and preferably 1 to 5 mg/ml (e.g. 1 to 4 mg/ml).

Long-term preservation of the drug held or supported by the matrix (drug holder or drug retainer) with main-
taining the activity of the drug can be assured by storing the drug under dry conditions. More concretely, preservation of the drug in dry condition may be accomplished by, for instance, a process which comprises efficiently drying the drug holder holding the drug, packaging the drug holder in a film having a small water permeability (e.g. an aluminum film) and vacuum sealing it. Further, in order to retain the dry condition the drug holder supporting the drug may be vacuum-sealed and packaged together with a desiccating agent or dryer (e.g. a zeolite-based desiccator such as "SELM"
 manufacture by Tokai Chemical Industries, Ltd., a silica gel-based desiccator, etc.). When the drug is oxidatively decomposed, an oxygen absorbent (e.g. "AGELESS" manufactured by Mitsubishi Gas Chemical Co., Ltd.) may be included in the package in addition to the desiccating agent.

[0081] The amount of the drug held relative to the matrix (drug holder) may only be an effective amount according to the species of the drug, species of the drug holder, area or portion to be administered, and is, for example, 0.1 to 100 µg, and preferably 0.5 to 50 µg (e.g. 1 to 50 µg) per 1 cm² of the sheet-like drug holder.

[0082] In the present invention, the interface for iontophoresis may be composed of the porous matrix holding or supporting the drug as mentioned above, or it may be composed of the porous matrix holding or supporting the drug and the humectant held or supported by the porous matrix.

It is noted that the drug is not necessarily held by the sheet-like matrix (e.g. a holder in the form of a membrane) but a solution containing the drug may be injected into the holder or neighborhood of the holder. In such a case, the interface may also be composed of the matrix and the humectant held or supported by the matrix. The drug may be included into the dissolution liquid, that is, the dissolution liquid may contain the humectant and the drug.

[0083] Furthermore, a suitable adsorption inhibitor may be incorporated into the dissolution liquid for dissolving the drug in order to ensure further inhibition of loss of the physiologically active peptide or protein due to adsorption. The adsorption inhibitor includes, for instance, an albumin (e.g. a bovine serum albumin (BSA), a human serum albumin (HSA) and other serum albumins), gelatin and other water soluble proteins; alkylbenzenesulfonic acid salts (e.g. a sodium salt) and other anionic surfactants, a <sub>8</sub> -20 alkyltrimethylammonium chloride, a <sub>8</sub> -20 alkyltrimethylammonium chloride, a <sub>8</sub> -20 alkylbenzyldimethylammonium chloride (benzalkonium chloride, hereinafter sometimes referred to as BAC), a 4-C<sub>1</sub> -10 alkylphenyloxyethoxyethylbenzyldimethylammonium chloride (e.g. benzethonium chloride) and other cationic surfactants, Tween 80 and other nonionic surfactants, and alkali metal salts (e.g. sodium chloride). The amount of the adsorption inhibitor may for example be 0.00001 to 1% (w/w), preferably 0.0001 to 0.5% (w/w), and more preferably 0.001 to 0.1% (w/w) based on the amount of the dissolution liquid. Further, an appropriate absorption accelerator (e.g. monoterpenes, aliphatic monoglyceride, Azone (manufactured by Nelson), limonen, oleic acid, lauric acid, octanol) may be incorporated into the drug dissolution liquid. The content of the absorption accelerator is, for instance, 0.1 to 80% (w/w), preferably 0.5 to 50% (w/w), and more preferably about 1 to 30% (w/w) based on the amount of the dissolution liquid.

[0084] The interface composed of the drug holder (porous body) is suitable for transdermal drug delivery (endermic drug administration) by iontophoresis using a variety of applicators which are applicable to a skin. The applicator is provided with an electrode to which an electric voltage is applied and an interface which is conductive to the electrode capable of contacting the skin, and holds or supports the drug. The applicator can be supplied with an aqueous solution for dissolving the drug containing the humectant. A transdermal drug delivery system comprises an interface composed of the matrix (in particular the sheet-like porous body), the humectant-containing a dissolution liquid for dissolving the drug, and a supply means for supplying the dissolution liquid to the interface. The drug dissolved with the dissolution liquid is transdermally or endermically absorbed by means of iontophoresis. Fig. 1 is a cross sectional view illustrating an embodiment of the applicator comprising the interface.

[0085] The applicator shown in Fig. 1 is provided with a support (base member) 4 having flexibility and being formed with an opening 9, and a container (reservoir) 3 disposed in a part corresponding to the opening 9. The container is provided with an electrode 1 such as a silver electrode, and accommodates an electric conductor 2 such as an electric conductive nonwoven fabric or sponge containing water or an electric conductive gel such as a water-containing gel, poly(vinyl alcohol) (PVA) comprising NaCl. The electric conductor 2 may comprise a porous sponge or nonwoven fabric containing an aqueous solution comprising a hydrophilic substance with water retention. Below of the support 4 corresponding to the opening 9 there is disposed an ion exchange membrane 5, the inner surface of which faces the electric conductor 2, and an interface 6 is laminated by means of an adhesive tape 7. The adhesive tape 7 is utilized for attaching the applicator to the skin. The electric conductor 2 of the container 3 is conductible to the electrode 1 and capable of contacting the ion exchange membrane 5 and interface 6 through opening 9. Further, an injection port 10 injecting a liquid is formed between the ion exchange membrane 5 and the interface 6.

[0086] When such an applicator is used in case that the interface holds or supports the drug a nozzle tip of an injection tip 8 may be inserted into the injection port 10 between the ion exchange membrane 5 and the interface 6 to inject the drug dissolution liquid such as a distilled water for injection containing the humectant. When the interface does not hold or support the drug, a solution containing the drug and the drug dissolution liquid containing the humectant may be injected into the interface 6. In a case that the interface holds or supports both the drug and the humectant the drug dissolution liquid such as a distilled water for injection may only be injected into the interface 6.
Comparative Example 1

EXAMPLES

Comparative Example 1

An abdominal skin of a male SD rat (7-week aged) was clipped with a hair clipper, treated with a shaver under
pentobarbital-anesthetization and cleaned with an absorbent cotton containing a 70% aqueous solution of ethanol for defatting and disinfection.

[0094] In the iontophoresis was used an applicator illustrated in Fig. 1. That is, the drug holder (Biodyne Plus Membrane, Nihon Pall Ltd., Japan; 2.5 cm²) was previously dipped in a 10% (w/v) bovine serum albumin (BSA) and dried to hold or possess 40 µg of hPTH (1→34) per membrane in dry condition and thereby an interface for iontophoresis was obtained. This interface was applied and fixed to the abdominal skin of the rat. After application of the interface to the skin, the dried drug was dissolved by supplying 120 µl of a distilled water from an injection tip 8 to the interface. The electric current application was effected by using a pulse direct current electric voltage of a direct-current 12-V constant voltage with a frequency of 40 kHz and an ON/OFF ratio of 3/7, and repeating three times a combination of 15-minutes current application and 5-minute-non-current application. This current application pattern was repeated three times with an interval of 2 hours. After a predetermined time lapse, blood was taken from jugular veins (cervical vein) of the rat and centrifuged at a rate of 12,000 rpm for 10 minutes to give a serum sample. The concentration (pg/ml) of the hPTH (1→34) in the serum was determined by radioimmunoassay method. The results are illustrated in Fig. 2. In Fig. 2, long narrow boxes in axis of abscissa (time) represent electric current application time.

Comparative Example 2

[0095] The hPTH (1→34) was transdermally administered in the same manner as Comparative Example 1 using the same interface for iontophoresis, administration process, conditions of current application and determination method of serum hPTH (1→34) concentration, except that 60 µl of a distilled water was supplied from the injection tip 8 immediately before the second and third current application cycles respectively. The results are set forth in Fig. 2.

Example 1

[0096] The hPTH (1→34) was administered in the same interface for iontophoresis, administration process, conditions for current application and determination method of serum hPTH (1→34) concentration as Comparative Example 1 except that 120 µl of a 30% (w/w) glycerin aqueous solution in lieu of the distilled water was injected once after adhesion of the interface. The results are shown in Fig. 2.

[0097] As apparent from Fig. 2, in the single supply of the distilled water (Comparative Example 1), third peak corresponding to the numbers of the current application cycles was not found, to the contrary, in the single supply of the 30% (w/w) glycerin aqueous solution (Example 1), three peaks corresponding to the current application cycles were found, equaling to the three times-supply of the distilled water (Comparative Example 2). The bioavailability (BA) was evaluated from the ratio of the area under the serum hPTH concentration-time curve (AUC value) of the tested group relative to the AUC value obtained by intravenous administration on same dose basis [actual intravenous dose, 2 µg/kg of hPTH (1→34)]. The BA was 17.8%, 9.0% and 13.8% for Example 1, Comparative Example 1 and Comparative Example 2 respectively. Thus, the single supply of 30% (w/w) aqueous solution of glycerin provides an equal absorptivity to the three times supply of the distilled water.

Example 2

[0098] By conducting a single injection of 120 µl of a 10% (w/w) aqueous solution of glycerin in lieu of the distilled water after application of the interface, the hPTH (1→34) was transdermally delivered in the same manner as Comparative Example 1 employing the same interface for iontophoresis, administration process and conditions for current application.

[0099] In the single supply of the 10% (w/w) aqueous solution of glycerin (Example 2), the bioavailability (BA) was 9.5%, as evaluated from the ratio of the area under the serum hPTH concentration-time curve (AUC value) of the tested group relative to the AUC value obtained by intravenous administration on same dose basis [actual intravenous dose, 2 µg/kg of hPTH (1→34)].

Example 3

[0100] Except that single injection of 120 µl of a 60% (w/w) aqueous solution of glycerin in lieu of the distilled water was conducted after application of the interface, the hPTH (1→34) was transdermally administered employing the same interface for iontophoresis, administration process and conditions of current application as Comparative Example 1.

[0101] In the single supply of the 60% (w/w) aqueous solution of glycerin (Example 3), the bioavailability (BA) was 18.5%, as evaluated from the ratio of the area under the serum hPTH concentration-time curve (AUC value) of the tested group relative to the AUC value obtained by intravenous administration on same dose basis [actual intravenous
Example 4

The hPTH (1→34) was transdermally administered in the same interface for iontophoresis, administration process and conditions for current application as Comparative Example 1, except that 120 µl of a 30% (w/w) aqueous solution of proline was once injected, instead of the distilled water, after application of the interface by using the same interface for iontophoresis, administration process and conditions for current application as Comparative Example 1. The results are illustrated in Fig. 3. The results of Comparative Example 2 are also shown in Fig. 3. In Fig. 3, narrow and long boxes in the axis of abscissa (time) denote current application time (period).

Example 5

Except that 120 µl of a 10% (w/w) aqueous solution of proline in lieu of the 30% (w/w) aqueous solution of proline was injected after application of the interface, the hPTH (1→34) was transdermally administered employing the same interface for iontophoresis, administration process and conditions of current application as Example 4. The results are set forth in Fig. 4. As apparent from Fig. 4, the single supply of the 10% (w/w) aqueous solution of proline provide a similar pattern of the hPTH (1→34) in serum to Example 1, and BA was 17.8%.

Example 6

The hPTH (1→34) was transdermally administered by employing the same interface for iontophoresis, administration process and conditions of current application as Example 4, except that 120 µl of 10% (w/w) aqueous solution of sodium pyroglutamate was injected in lieu of the 30% (w/w) aqueous solution of proline after application of the interface. The results are shown in Fig. 4. As clearly illustrated in Fig. 4, a single supply of the 10% (w/w) aqueous solution of sodium pyroglutamate resulted in a similar pattern of the hPTH (1→34) in blood to Example 1, and BA was 15.2%.

Claims

1. An interface (6) for iontophoresis comprising a matrix for holding or supporting a drug in a drug dissolution liquid comprising a humectant characterised in that the matrix is a porous matrix.

2. The interface (6) as claimed in claim 1, wherein the humectant is at least one member selected from the group consisting of polyhydric alcohols, sugar alcohols, amino acids and acidic mucopolysaccharides.

3. The interface (6) as claimed in claim 1, wherein the content of the humectant is 1 to 90% by weight, based on the amount of the drug dissolution liquid.

4. The interface (6) as claimed in claim 2, wherein the polyhydric alcohol contains 2 to 4 hydroxyl-groups per molecule.

5. The interface (6) as claimed in claim 4, wherein the polyhydric alcohol is glycerin.

6. The interface (6) as claimed in claim 2, wherein the amino acid contains a nitrogen-containing heterocycle.

7. The interface (6) as claimed in claim 2, wherein the amino acid is a non-aromatic nitrogen-containing 5-membered heterocycle.

8. The interface (6) as claimed in claim 2, wherein the amino acid is proline or hydroxyproline.

9. The interface (6) as claimed in claim 2, wherein the concentration of the polyhydric alcohol is 10 to 50% per weight.

10. The interface (6) as claimed in claim 2, wherein the concentration of the amino acid is 1 to 30% by weight.
11. The interface (6) as claimed in claim 1, wherein the drug is (1) a physiologically active peptide or protein, or (2) a non-peptide physiologically active compound.

12. The interface (6) as claimed in claim 1, wherein the drug is (1) a physiologically active peptide or protein with a molecular weight of 100 to 30,000, or (2) a non-peptide physiologically active compound with a molecular weight of 100 to 1,000.

13. Use of a humectant in iontophoresis for promoting transdermal absorption of a drug held or supported by an interface (6), wherein the interface comprises porous matrix.

14. The use of claim 13 characterised in that a dissolution liquid comprising the humectant is used for dissolving the drug.

15. The use as claimed in claim 13, wherein the humectant is at least one member selected from the group consisting of polyhydric alcohols, sugar alcohols, amino acids and acidic mucopolysaccharides.

16. The use as claimed in claim 15, wherein the polyhydric alcohol contains 2 to 4 hydroxyl-groups per molecule.

17. The use as claimed in claim 15, wherein the polyhydric alcohol is glycerin.

18. The use as claimed in claim 15, wherein the amino acid contains a nitrogen-containing heterocycle.

19. The use as claimed in claim 15, wherein the amino acid is a non-aromatic nitrogen-containing 5-membered heterocycle.

20. The use as claimed in claim 15, wherein the amino acid is proline or hydroxyproline.

21. The use as claimed in claim 13, wherein the drug is (1) a physiologically active peptide or protein, or (2) a non-peptide physiologically active compound.

22. The use as claimed claim 13, wherein the drug is (1) a physiologically active peptide or protein with a molecular weight of 100 to 30,000, or (2) a non-peptide physiologically active compound with a molecular weight of 100 to 1,000.

Patentansprüche

1. Grenzfläche (6) für die Iontophorese, umfassend eine Matrix zum Halten oder Stützen eines Wirkstoffs in einer Wirkstoffauflösungsflüssigkeit, die ein Feuchthaltemittel umfasst, dadurch gekennzeichnet, dass die Matrix eine poröse Matrix ist.

2. Grenzfläche (6) gemäß Anspruch 1, wobei das Feuchthaltemittel wenigstens eine Verbindung ist, die aus der Gruppe ausgewählt ist, bestehend aus mehrwertigen Alkoholen, Zuckeralkoholen, Aminosäuren und sauren Mucopolysacchariden.

3. Grenzfläche (6) gemäß Anspruch 1, wobei der Gehalt des Feuchthaltemittels 1 bis 90 Gew.-% ist, bezogen auf die Menge der Wirkstoffauflösungsflüssigkeit.

4. Grenzfläche (6) gemäß Anspruch 2, wobei der mehrwertige Alkohol 2 bis 4 Hydroxygruppen pro Molekül enthält.

5. Grenzfläche (6) gemäß Anspruch 4, wobei der mehrwertige Alkohol Glycerin ist.

6. Grenzfläche (6) gemäß Anspruch 2, wobei die Aminosäure einen stickstoffhaltigen Heterocyclus enthält.

7. Grenzfläche (6) gemäß Anspruch 2, wobei die Aminosäure ein fünfgliedriger Heterocyclus ist, der keinen aromatischen Stickstoff enthält.

8. Grenzfläche (6) gemäß Anspruch 2, wobei die Aminosäure Prolin oder Hydroxyprolin ist.

10. Grenzfläche (6) gemäß Anspruch 2, wobei die Konzentration der Aminosäure 1 Gew.-% bis 30 Gew.-% ist.

11. Grenzfläche (6) gemäß Anspruch 1, wobei der Wirkstoff (1) ein physiologisch aktives Peptid oder Protein oder (2) eine physiologisch aktive Nicht-Peptid-Verbindung ist.

12. Grenzfläche (6) gemäß Anspruch 1, wobei der Wirkstoff (1) ein physiologisch aktives Peptid oder Protein mit einer Molmasse von 100 bis 30 000 oder (2) eine physiologisch aktive Nicht-Peptid-Verbindung mit einer Molmasse von 100 bis 1000 ist.

13. Verwendung eines Feuchthaltemittels in der Iontophorese, um die transdermale Absorption eines Wirkstoffs zu fördern, der durch eine Grenzfläche (6) gehalten oder gestützt wird, wobei die Grenzfläche eine poröse Matrix umfasst.


15. Verwendung gemäß Anspruch 13, wobei das Feuchthaltemittel wenigstens eine Verbindung ist, die aus der Gruppe ausgewählt ist, bestehend aus mehrwertigen Alkoholen, Zuckeralkoholen, Aminosäuren und sauren Mucopolysacchariden.


17. Verwendung gemäß Anspruch 15, wobei der mehrwertige Alkohol Glycerin ist.

18. Verwendung gemäß Anspruch 15, wobei die Aminosäure einen stickstoffhaltigen Heterocyclus enthält.

19. Verwendung gemäß Anspruch 15, wobei die Aminosäure ein fünfgliedriger Heterocyclus ist, der keinen aromatischen Stickstoff enthält.

20. Verwendung gemäß Anspruch 15, wobei die Aminosäure Prolin oder Hydroxyprolin ist.

21. Verwendung gemäß Anspruch 13, wobei der Wirkstoff (1) ein physiologisch aktives Peptid oder Protein oder (2) eine physiologisch aktive Nicht-Peptid-Verbindung ist.

22. Verwendung gemäß Anspruch 13, wobei der Wirkstoff (1) ein physiologisch aktives Peptid oder Protein mit einer Molmasse von 100 bis 30 000 oder (2) eine physiologisch aktive Nicht-Peptid-Verbindung mit einer Molmasse von 100 bis 1000 ist.

Revendications

1. Interface (6) pour iontophorèse, comprenant une matrice pour maintenir ou supporter un médicament dans un liquide dissolvant le médicament, comprenant un humidifiant, caractérisé en ce que la matrice est une matrice poréuse.

2. Interface (6) suivant la revendication 1, dans laquelle l'humidifiant est au moins un membre choisi parmi le groupe consistant en des alcools polyhydroxylés, des alcools de sucre, des acides aminés et des mucopolysaccharides acides.

3. Interface (6) suivant la revendication 1, dans laquelle la teneur en humidifiant se situe dans l'intervalle allant de 1 à 90% en poids, sur base de la quantité de liquide dissolvant le médicament.

4. Interface (6) suivant la revendication 2, dans laquelle l'alcool polyhydroxylé contient 2 à 4 radicaux hydroxylé par molécule.
5. Interface (6) suivant la revendication 4, dans laquelle l'alcool polyhydroxylé est la glycérine.

6. Interface (6) suivant la revendication 2, dans laquelle l'acide aminé contient un hétérocyle azoté.

7. Interface (6) suivant la revendication 2, dans laquelle l'acide aminé est un hétérocyle à 5 membres, azoté, non aromatique.

8. Interface (6) suivant la revendication 2, dans laquelle l'acide aminé est la proline ou l'hydroxyproline.

9. Interface (6) suivant la revendication 2, dans laquelle la concentration en alcool polyhydroxylé se situe dans l'intervalle allant de 1 à 50% en poids.

10. Interface (6) suivant la revendication 2, dans laquelle la concentration en acide aminé se situe dans l'intervalle allant de 1 à 30% en poids.

11. Interface (6) suivant la revendication 1, dans laquelle le médicament est (1) un peptide physiologiquement actif ou une protéine, ou (2) un composé non peptidique physiologiquement actif.

12. Interface (6) suivant la revendication 1, dans laquelle le médicament est (1) un peptide physiologiquement actif ou une protéine ayant un poids moléculaire allant de 100 à 30 000, ou (2) un composé non peptidique physiologiquement actif ayant un poids moléculaire allant de 100 à 1000.

13. Utilisation d'un humidifiant en iontophorèse, pour favoriser l'absorption transdermique d'un médicament maintenu ou supporté par une interface (6), où l'interface comprend un matériau poreux.

14. Utilisation suivant la revendication 13, caractérisée en ce qu'un liquide dissolvant comprenant un humidifiant est utilisé pour dissoudre le médicament.

15. Utilisation suivant la revendication 13, dans laquelle l'humidifiant est au moins un membre choisi parmi le groupe consistant en des alcools polyhydroxylés, des alcools de sucre, des acides aminés et des mucopolysaccharides acides.

16. Utilisation suivant la revendication 15, dans laquelle l'alcool polyhydroxylé contient 2 à 4 radicaux hydroxyde par molécule.

17. Utilisation suivant la revendication 15, dans laquelle l'alcool polyhydroxylé est la glycérine.

18. Utilisation suivant la revendication 15, dans laquelle l'acide aminé contient un hétérocyle azoté.

19. Utilisation suivant la revendication 15, dans laquelle l'acide aminé est un hétérocyle à 5 membres, azoté, non aromatique.

20. Utilisation suivant la revendication 15, dans laquelle l'acide aminé est la proline ou l'hydroxyproline.

21. Utilisation suivant la revendication 13, dans laquelle le médicament est (1) un peptide physiologiquement actif ou une protéine, ou (2) un composé non peptidique physiologiquement actif.

22. Utilisation suivant la revendication 13, dans laquelle le médicament est (1) un peptide physiologiquement actif ou une protéine ayant un poids moléculaire allant de 100 à 30 000, ou (2) un composé non peptidique physiologiquement actif ayant un poids moléculaire allant de 100 à 1000.
FIG. 3

- ● Example 4
- ○ Comp. Ex. 2

Serum hPTH (1–34) concentration (pg/mL) vs. Time course (minute)
FIG. 4.

Serum hPTH (1–34) concentration (pg/ml)

- Example 5
- Example 6

Time course (minute)