EUROPEAN PATENT SPECIFICATION

Date of publication of patent specification: 20.07.94

Int. Cl.: A61M 5/14

Application number: 90108404.6

Date of filing: 04.05.90

Vent for flashback plug.

Priority: 11.05.89 US 350960

Date of publication of application: 14.11.90 Bulletin 90/46

Publication of the grant of the patent: 20.07.94 Bulletin 94/29

Designated Contracting States: AT BE CH DE DK ES FR GB GR IT LI LU NL SE

References cited:
GB-A- 1 243 369
US-A- 3 859 998
US-A- 4 722 344

Proprietor: Becton Dickinson and Company
One Becton Drive
Franklin Lakes New Jersey 07417-1880(U.US)

Inventor: Mersch, Steve Henry
7347 Weaver Road
Germantown, Ohio (US)
Inventor: Spielvogel, David Ellwood
45 Graham Road
Springboro, Ohio (US)
Inventor: Daugherty, Charles William
1726 Paintersville New Jasper Road
Xenia, Ohio (US)

Representative: Dalimeyer, Georg et al
Patentanwälte
von Kreisler-Selting-Werner
Postfach 10 22 41
D-50462 Köln (DE)

Note: Within nine months from the publication of the mention of the grant of the European patent, any person may give notice to the European Patent Office of opposition to the European patent granted. Notice of opposition shall be filed in a written reasoned statement. It shall not be deemed to have been filed until the opposition fee has been paid (Art. 99(1) European patent convention).
Description

This invention relates to intravenous needle assemblies and, more particularly, to a plug usable with an intravenous needle for detecting the presence of the needle point within a blood vessel, and for preventing flow of blood from the assembly during the venous puncture procedure. The device provides for venting air rapidly, in order to enable the blood to flow from the blood vessel into a transparent blood-detecting chamber under venous pressure and in some cases more rapidly, than has been the case in the past, while at the same time preventing any blood flow through the vent passages.

The preamble of claim 1 starts from prior art according to US-A-3859998.

During the placement of a needle or flexible catheter into a vein or other body member, it is desirable to determine whether or not the tip of the needle or catheter is properly situated within the vessel. Because the introduction of the assembly into the vein is normally accomplished by the use of an opaque rigid metallic needle, it is impossible to detect the presence of blood in the needle and needle hub.

Because of this, prior art introducer needles are equipped with a hub having a transparent flash chamber into which the blood flows to indicate that the needle point is properly placed. Many such devices, however, have leakage problems which cause blood flow over the hands of the user. It is important to avoid such circumstances, because of the potential for transfer of disease in exposure to blood from a patient. In providing a chamber with means for venting air therefrom so that the blood will flow rapidly into the chamber for indication of venous entry, the air vents, have a tendency to leak.

This disadvantage is inherent in the plug arrangement according to US-A-3859998, being provided with a thin diaphragm at the distal end of the plug. A slit is formed in the diaphragm by cutting without removal of material. Even if the slit is extremely small the flexible lips may be unable to return to their sealing position after opening for venting air and blood leaks through the vent passage.

With this invention as claimed, by contrast, a flashback assembly is provided with transparent walls to indicate the presence of blood in the hub of the assembly and that the needle has, indeed, entered the vein of a patient, with the vent being comprised of a required cross-section of actual venting area, but with vent holes much smaller than those achieved in the prior art. This is arranged in accordance with this invention by the use of a laser for drilling the vent holes according to claim 1. By doing so, the laser provides the same or a greater cross-sectional area of actual air venting, while at the same time providing holes which are small enough to prevent the leakage of blood through the air vents.

In accordance with this invention, a laser is used for drilling one or an array of small holes in the end of the flow control plug. The hole or holes comprise a total sufficient cross-sectional area to provide flashback times at least equivalent or better than the prior art plugs utilizing other conventional venting methods such as membranes, sintered thermoplastics, or slit valves.

The laser utilized for drilling the holes may be, for example, a YAG laser (yttrium-aluminum-garnet). Also, a ruby laser may be utilized, but the YAG laser is preferred. The holes will have a diameter of less than 50.8μm (0.002 inches) and, preferably, less than 25.4μm (0.001 inch). In this connection, it has been determined that holes of 76.2μm (0.003 inches) or above in diameter leak blood at venous pressures.

In considering generally the conditions for carrying out the invention herein, it has been determined that conventional thermoplastic materials such as polyethylene do not absorb the laser beam wave length to the level required for producing the holes in accordance herewith, without containing an additive which increases absorption. Thus, it was found in accordance with this invention that an additive such as ACRA-WAX® added to the material under consideration provides the proper absorption characteristics for plugs made in accordance with this invention. That is, it is important that when the holes are being drilled a proper level or degree of absorption of a laser wave length takes place in order to achieve vaporization of the material, and, hence, properly drilled holes. If the proper level is not obtained, melting of the material takes place with clogging of such small holes.

Thus, pellets of polyethylene were provided with a one percent quantity, by weight, of ACRA-WAX® and extruded into ribs of about 127μm (0.005 inches) thick. Circular samples of this material were drilled with the YAG laser. A sample with three holes drilled in the sample with each hole of less than 50.8μm (0.002 inches) in diameter were tested utilizing a dyed water to indicate the presence of the liquid in the plug of the invention. The test indicated not only rapid flashback time but an absence of leakage.

In considering further the conditions for carrying out the invention here, the following thermoplastic materials are representative of materials which may be utilized for formulating the plugs of the invention. These materials are polyethylene as indicated above, polypropylene, polyvinyl chloride, acrylonitrile-butadiene-styrene terpolymer, polyeth-
ylene terephthalate and polyurethane. It will be understood that other materials may be used as long as they come within the operating parameters discussed herein. While most materials listed above will not have the appropriate absorption requirement necessary for laser drilling as discussed herein, it should be understood that some materials will, indeed, have those characteristics, thus eliminating the need for an additive for that purpose.

Examples of additives which may be used to increase the absorption properties of the thermoplastics utilized with the invention here include ADVAWAX® 280, a product of Morton Thiokol, or ACRA-WAX® C lubricant, a product of Glyco Incorporated, 488 Main Street, P.O. Box 5100 Norwalk, Connecticut 06856. ACRA-WAX is an alkyl amide which is the reaction product of ethylene diamine and stearic acid. The specific name is N,N'-ethylene bis (stearamide). The additive may be mixed with the resin at the rate of within the range of between about 0.5 and 5 percent by weight, and, preferably, within the range of between about 1.0 and 3.0 percent by weight.

In order to prepare the plugs of the invention, the following example indicates one representative procedure for making such plugs.

EXAMPLE

Polyethylene pellets (Eastman 1870A) were melt processed and mixed with 1.0 percent ACRAWAX®, using a twin screw extruder/pelletizer. After drying, the pellets were molded into the desired plug shape. The appropriate size and number of holes were then drilled using a YAG laser as discussed above. In this connection the wall of the plug to be drilled was arranged to have in the area where the holes are to be drilled an even unvarying width of about 127µm (0.005 inches) in thickness. Subsequently, the holes, as discussed above, were drilled by the laser in this wall portion.

Other objects and advantages of this invention will be apparent from the following description, the accompanying drawings and the appended claims.

Fig. 1 is an exploded perspective view of an intravenous needle assembly showing the plug of the present invention in a position removed from the end of the blood-detecting chamber; Fig. 2 is a longitudinal cross-sectional view of the needle assembly of Fig. 1 showing the plug of the invention inserted within the blood-detecting chamber; and Fig. 3 is an end view of the plug as viewed from the left in Fig. 2.

Referring to the drawings in which like reference characters refer to like parts throughout the several views thereof, Figs. 1 and 2 illustrate the vent plug of the invention as used in an intravenous needle assembly as shown generally at 10. The assembly includes an introducer needle 15 which is in the form of a hollow hypodermic needle having a point 14 on one end thereof. Needle 15 is secured at its blunt end to a plastic hub 12 which has a transparent blood-detecting chamber 20 integral with its proximal end. The entire hub and blood-detecting chamber assembly may, preferably, be molded in one piece from a suitable clear plastic material.

In the preferred embodiment, needle 15 serves the function of introducing a flexible plastic catheter 18 into a vein or other body vessel. Catheter 16 is attached to a hub 18 at its proximal end, and hub 18 is adapted to be removably secured to a fitting 32 on the distal end of hub 12.

The present invention eliminates the necessity for any complex form of operation necessary to indicate venous entry and provides a relatively simple, one-piece plug which performs the function of rapid indication of venous entry. This is achieved with the plug of the invention by having an increased cross-sectional vent area combined for venting air from the plug, so that when venous entry is made the blood flows rapidly into and fills up the transparent chamber in the hub of the assembly, as discussed herein. Nevertheless, the individual holes are of such small dimension that blood will not flow through them so that there is no contamination to the user of the device by the blood of a patient upon which the assembly of the invention is being utilized. This reduces the exposure to AIDS, hepatitis or other diseases carried by the blood of patients, for example.

The plug of the invention is shown generally in Fig. 1 at 22 and includes a substantially cylindrical body portion 24 having extending from the front end thereof, a neck portion 27. As can be seen in Fig. 2, neck portion 27 includes an internal cylindrical passage 26. The front face 30 of neck portion 27 is a wall of substantially even thickness, as discussed above. The wall 30 is formed so that it has a thickness of around 127µm (0.005 inches) in order to be appropriate for receiving a plurality or laser drilled openings 28. As discussed above, laser openings 28 are drilled to have a diameter of less than 50,8µm (0.002 inches) and preferably 25,4µm (0.001 inch).

The number of laser drilled holes 28 provided will depend upon the dimension of the assembly being utilized and the volume of air required to be vented through holes 28 from the transparent chamber 20, so that when the point 14 of needle 15 is inserted into the vein of a patient blood will flow rapidly back through needle 15 into the transparent chamber 20. This happens because the air under venous pressure moves rapidly through vent holes 28. As can be seen in Fig. 3, three such vent
holes 28 are shown. However, a greater number may be selected, as discussed above, depending upon the desired properties for the individual plug being formulated.

To initiate the introduction of a needle into a vein, in accordance with the unit of the invention herein, the unit is fully assembled as shown in Fig. 2 with catheter 16 positioned over needle 15 and with plug 22 firmly seated into the rear or proximal end of blood-detecting chamber 20. The introduction of the needle point 14 into a vein causes blood to flow through the hollow needle and into the blood detecting chamber 20.

Air contained within the hollow needle and the blood-detecting chamber will be forced by the blood through the vent holes 28 out into the atmosphere. Obviously, blood flowing into chamber 20 will be detected by the operator through the transparent wall thereof. Because of the extremely small size of the vent holes 28, blood will be retained within the chamber and not permitted to pass to the passage 26 in plug 22. Thereafter, when it is desired to attach an administration set or other device to the catheter hub, it is only necessary to withdraw the needle from the catheter and thereby, expose the open female luer end of hub 18 for the appropriate male fitting.

Alternatively, needle 15 may be used independently of catheter 16 and an administration set or other device may be attached directly to the blood-detecting chamber 20 by merely removing plug 22 therefrom.

As will be apparent from the foregoing, the invention herein provides an effective device for detecting the presence of an introducer needle point within the vein of a patient and for preventing the loss of blood from the needle assembly. Moreover, the device of the invention may be made with relatively inexpensive materials and known conventional equipment which makes the plug of the invention particularly appropriate for mass production techniques and reduced cost.

While the form of apparatus herein described constitutes a preferred embodiment of the invention, it is to be understood that the invention is not limited to the precise form of apparatus shown, and that changes may be made therein without departing from the scope of the invention which is defined in the appended claims. For example, as discussed previously, a greater or lesser number of holes may be drilled by the laser beam with the limitation only being the requirement for the particular plug dimensions being utilized. Moreover, a wide variety or selection of thermoplastic materials may be utilized provided the appropriate additive is selected, when required, in the proper quantity in order to increase absorption of the laser beam wavelength appropriately to the level required for vaporization of the material being worked upon as opposed to melting that material. That is, in order to provide effective holes of such small dimension, it is necessary for the material to be vaporized. If the material melts then the proper holes will not be provided in such small dimensions.

Alternatively, as will be understood by practitioners-in-the-art materials may be selected which have sufficient absorption characteristics so that an additive is not required.

Claims

1. A plug for use in plugging the proximal end of a transparent flashback chamber (20) in an intravenous needle assembly, said plug (22) for providing air venting of said flashback chamber (20) comprising
   a) a hollow body (24) defining an air vent passage;
   b) a hollow neck portion (27) positioned on the distal end of said body (24), said neck portion (27) being integral with said body portion (24);
   c) a front face (30) on the distal end of said neck portion (27); and
   d) said front face (30) being thin-walled and of the same thickness throughout and being provided with a vent passage, characterized in that the vent passage consists of a plurality of vent holes (28) in said front face (30); said vent holes (28) being laser drilled and having a diameter less than 50.8 \( \mu \)m (0.002 inches) and at least said thin-walled front face (30) being comprised of a thermoplastic material having sufficient laser absorption characteristics to vaporize under the effect of a laser beam, so as to create said vent holes (28).

2. The plug of claim 1, further characterized by
   a) said plug (22) being comprised of a material selected from the group consisting of polyethylene, polypropylene, polyvinyl chloride, acrylonitrilebutadiene-styrene terpolymer, polyethylene terephthalate, polyurethane and mixtures thereof.

3. The plug of claim 1, further characterized by
   a) said front face (30) having a thickness of about 127 \( \mu \)m (0.005 inches).

4. The plug of claims 1 to 3, further characterized by
   a) said thin-walled front face (30) having in percent by weight an amount of an additive effective for optimizing said vaporization.
5. The plug of claim 4, further characterized by:
   a) said additive is present in percent by
      weight within the range of between about
      0.5 and 5 percent.

6. The plug of claim 4, further characterized by
   a) said additive is a reaction product of
      ethylene diamine and stearic acid.

7. The plug of claim 6, further characterized by
   a) said additive is N,N'-ethylene bis
      (stearamide).

8. An intravenous needle assembly (10) comprising
   a) a hollow pointed needle (15);
   b) a hub (12) secured to the proximal end of
      said needle (15);
   c) said hub (12) having a transparent blood-
      detecting chamber (20);
   d) a plug (22) being removably secured in
      said chamber (20) for venting air from said
      transparent blood-detecting chamber (20)
      characterized by
      the said plug (22) being according to claims 1
      to 7.

9. A process for manufacturing a plug according to
    claims 1 to 7, being provided with a hollow
    neck portion (27) having a front face (30) that
    comprises a vent passage,
    characterized by
    molding at least the thin-walled front face (30)
    of a thermoplastic material having sufficient
    laser absorption characteristics to vaporize un-
    der the effect of a laser beam and
    then drilling the appropriate number of vent
    holes (28) having a size of less than 50.8µm
    (0.002 inches) into the front face (30) using a
    laser.

Patentansprüche

1. Stopfen zum Schließen des proximalen Endes
   einer transparenten Rückflußkammer (20) einer
   intravenösen Nadelanordnung, wobei der zum
   Lüften der Rückflußkammer (20) vorgesehene
   Stopfen (22) aufweist:
   a) einen Hohlkörper (24), der einen Lüf-
      tungsduchlaß bildet;
   b) einen am distalen Ende des Körpers (24)
      angeordneten hohlen Halsteil (27), wobei
      das Halsteil (27) einstückig mit dem Körper
      (24) ausgebildet ist;
   c) eine Vorderfläche (30) am distalen Ende
      des Halsteils (27); und
   d) wobei die Vorderfläche (30) dünnwandig,
      durchgehend gleich dick und mit einem Lüf-
      tungsduchlaß versehen ist,
   dadurch gekennzeichnet, daß
   - der Lüftungsduchlaß aus mehreren Lüf-
      tungslochern (28) in der Vorderfläche
      (30) besteht;
   - die Lüftungslocher (28) laseroberholt
      sind und einen Durchmesser von weniger
      als 50.8µm (0.002 Inch) aufweisen, und
   - wenigstens die dünnwandige Vorderflä-
      che (30) aus einem thermoplastischen
      Material mit Laserabsorptionseigenschaf-
      ten besteht, die ausreichen, ein Ver-
      dampfen unter Einwirkung eines Laser-
      strahls zur Bildung der Lüftungslocher
      (28) zu bewirken.

2. Stopfen nach Anspruch 1, ferner dadurch ge-
   kennzeichnet, daß
   a) der Stopfen (22) aus einem Material ge-
      bildet ist, das aus der Gruppe bestehend
      aus Polyethylen, Polypropylen, Polyvinyl-
      chlorid, Acrylnitril/Butadien/Styrol-Terpolyme-
      rer, Polyethylenterephthalat, Polyurethan
      und Mischungen aus diesen gewählt ist.

3. Stopfen nach Anspruch 1, ferner dadurch ge-
   kennzeichnet, daß
   a) die Vorderfläche (30) eine Dicke von ungefähr
      127µm (0.005 Inch) aufweist.

4. Stopfen nach einem der Ansprüche 1 bis 3, ferner
   dadurch gekennzeichnet, daß
   a) die dünnwandige Vorderfläche (30) einen
      Gewichtsprozentanteil eines Additivs zur
      Optimierung des Verdampfens aufweist.

5. Stopfen nach Anspruch 4, ferner dadurch ge-
   kennzeichnet, daß
   a) das Additiv in einem Gewichtsprozentbe-
      reich zwischen ungefähr 0,5 und 5 Prozent
      vorliegt.

6. Stopfen nach Anspruch 4, ferner dadurch ge-
   kennzeichnet, daß
   a) das Additiv ein Reaktionsprodukt aus Ethyl-
      endiamin und Stearinäsäre ist.

7. Stopfen nach Anspruch 6, ferner dadurch ge-
   kennzeichnet, daß
   a) das Additiv N,N'-Ethilen bis (Stearamid)
      ist.

8. Intravenöse Nadelanordnung (10) mit
   a) einer hohlen spitzen Nadel (15);
   b) einem am proximalen Ende der Nadel
      (15) angebrachten Ansatz (12);
   c) wobei der Ansatz (12) eine transparente
      Bluterkennungskammer (20) aufweist;
d) un corps creux (24) définissant un passage d’évent;

(b) une partie en forme de col creux (27) disposée sur l’extrémité distale dudit corps (24), ladite partie de col (27) étant réalisée d’un seul tenant avec ladite partie de corps (24);

(c) une face avant (30) à l’extrémité distale de ladite partie de col (27); et

(d) ladite face avant (30) étant à paroi mince et d’épaisseur totalement uniforme, et comportant un passage d’évent, caractérisé en ce que le passage d’évent comprend une pluralité de trous d’évent (28) dans ladite face avant (30); lesdits trous d’évent (28) sont percés au laser et ont un diamètre inférieur à 50,8 μm (0,002 pouce), et que, au moins, ladite face avant à paroi mince (30) est composée d’une matière thermoplastique possédant des caractéristiques d’absorption du rayon laser suffisantes pour se vaporiser sous l’effet d’un faisceau laser, de manière à créer lesdits trous d’évent (28).

2. Le bouchon selon la revendication 1, caractérisé en ce que :
(a) ledit bouchon (22) est composé d’un matériau choisi dans le groupe comprenant le polyéthylène, le polypropylène, le chlorure de polyvinyle, le terpolymer de acrylonitrile-butadiène-styène, le polyéthylène tétraphthalate, le polyuréthane et leurs mélanges.

3. Le bouchon selon la revendication 1, caractérisé en outre en ce que :
(a) ladite face avant (30) possède une épaisseur d’environ 127 μm (0,005 pouce).

4. Le bouchon selon les revendications 1 à 3, caractérisé en outre en ce que :
(a) ladite face avant à paroi mince (30) comprend, en pourcentage en poids, une quantité d’additif adéquate pour optimiser ladite vaporisation.

5. Le bouchon selon la revendication 4, caractérisé en outre en ce que :
(a) ledit additif est présent, en pourcentage en poids, dans la gamme entre environ 0,5 et 5 pourcent.

6. Le bouchon selon la revendication 4, caractérisé en outre en ce que :
(a) ledit additif est un produit de réaction de l’éthylène diamine et de l’acide stéarique.

7. Le bouchon selon la revendication 6, caractérisé en outre en ce que :
(a) ledit additif est du N,N’-éthylène bis (stéaramide).

8. Un ensemble d’aiguille intraveineuse (10) comprenant
(a) une aiguille pointue creuse (15);
(b) un cône (12), fixé sur l’extrémité proximale de ladite aiguille (15);
(c) ledit cône (12) comprenant une chambre de détection de sang transparente (20);
(d) un bouchon (22) fixé de manière amovible sur ladite chambre (20) pour purger l’air de ladite chambre de détection de sang transparente (20), caractérisé en ce que ledit bouchon (22) est conforme aux revendications 1 à 7.

9. Un procédé de fabrication d’un bouchon selon les revendications 1 à 7, pourvu d’une partie en forme de col creux (27) pourvue d’une face avant (30) comprenant un passage d’évent, caractérisé par le moulage d’au moins la face
avant à paroi mince (30) en matière thermo-plastique possédant des caractéristiques d'absorption du rayon laser suffisantes pour se vaporiser sous l'effet d'un faisceau laser, et ensuite, le moulage du nombre approprié de trous d'évent (28) d'une dimension inférieure à 50,8 μm (0,002 pouce) dans la face avant (30) à l'aide d'un laser.